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Figure of Merit for CRISPR-Based Nucleic Acid-Sensing Systems: Improvement Strategies and Performance Comparison

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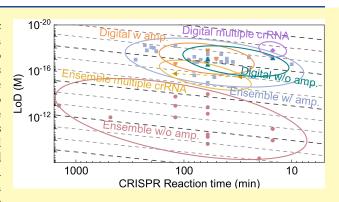




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ABSTRACT: Clustered regularly interspaced short palindromic repeats (CRISPR)-based nucleic acid-sensing systems have grown rapidly in the past few years. Nevertheless, an objective approach to benchmark the performances of different CRISPR sensing systems is lacking due to the heterogeneous experimental setup. Here, we developed a quantitative CRISPR sensing figure of merit (FOM) to compare different CRISPR methods and explore performance improvement strategies. The CRISPR sensing FOM is defined as the product of the limit of detection (LOD) and the associated CRISPR reaction time (T). A smaller FOM means that the method can detect smaller target quantities faster. We found that there is a tradeoff between the LOD of the assay and the required reaction time. With the proposed CRISPR sensing FOM, we evaluated five



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strategies to improve the CRISPR-based sensing: preamplification, enzymes of higher catalytic efficiency, multiple crRNAs, digitalization, and sensitive readout systems. We benchmarked the FOM performances of 57 existing studies and found that the effectiveness of these strategies on improving the FOM is consistent with the model prediction. In particular, we found that digitalization is the most promising amplification-free method for achieving comparable FOM performances (~1 fM·min) as those using preamplification. The findings here would have broad implications for further optimization of the CRISPR-based sensing. KEYWORDS: CRISPR, nucleic acid sensing, Cas proteins, figure of merit, limit of detection

C ensitive, accurate, and fast diagnostics of infectious diseases is crucial to optimize clinical care and guide infection control and public health interventions to limit disease spread. The development of the clustered regularly

interspaced short palindromic repeats (CRISPR)-based methods have taken center stage in biotechnology since the modified CRISPR/Cas9 system was applied for gene editing in mammalian genomes. Additionally, the CRISPR-Cas9 system has shown outstanding competence in nucleic acid sensing with high specificity.²⁻⁷ Recently, the discovery of the collateral cleavage in other Cas proteins like Cas12,8 Cas13,5 and Cas14¹⁰ made it possible to translate the sequence-specific targeting to other detectable signals, which has led to the increasing emergence of CRISPR-mediated biosensors. 9,11-21 In 2017, Gootenberg et al. introduced the specific highsensitivity enzymatic reporter unlocking (SHERLOCK), which exploits Cas13a for viral RNA detection. Simultaneously a Cas12a-based nucleic acid-sensing tool called an one-hour lowcost multipurpose highly efficient system (HOLMES) was introduced in 2018.8 The potential of CRISPR-based diagnostic systems was established in the recent global pandemic, where numerous CRISPR-based tests were

developed for severe acute respiratory syndrome coronavirus

2 (SARS-CoV-2) (emerging virus responsible for COVID-19 pneumonia) detection.²²·

While CRISPR-based nucleic acid-sensing systems are growing rapidly, an objective approach to benchmark and compare the performances of different systems remains challenging. Several previous studies have reviewed the performances of various CRISPR-based methods.^{32–36} As a potential diagnostic tool, two of the most important performance metrics in CRISPR-based methods are the achievable limits of detections (LODs) and the required reaction times.^{32,33} It is generally favorable to obtain lower LODs in shorter reaction times. Ramachandran et al. recently presented an analytical model based on Michaelis-Menten enzyme kinetics to address the question of what are the achievable limits of detection and associated CRISPR reaction times.³ This study demonstrated that the reaction time is inversely

Received: January 4, 2022 Accepted: February 22, 2022 Published: March 3, 2022





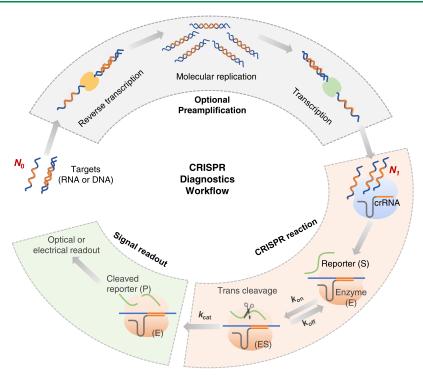


Figure 1. Typical steps in the CRISPR-based nucleic acid-sensing system. As an optional step, the DNA or RNA targets could be preamplified before the Cas reaction to increase the target quantity. Reverse transcription or transcription will be needed depending on the Cas protein property and targets (note that the illustration shows a Cas13 assay as an example). In the CRISPR reaction, the target molecules are specifically recognized and bounded to the Cas proteins and their associated crRNA (*i.e.*, Cas proteins activation). The trans-cleavage of the reporters could be described as an enzymatic reaction, where activated Cas proteins and reporters act as enzymes and substrates, respectively. The cleaved reporter results in signal development in various forms (optical or electrical), which is detected by a readout system.

proportional to the target abundance and the Cas enzyme catalytic efficiency. Nevertheless, from the whole system perspective, the achievable LOD and the associated reaction time depend not only on the Cas protein catalytic efficiency but also on other conditions such as preamplification, reaction volumes, ^{38,39} target activator, ^{8,37} and readout systems. ^{35,40} Due to these variations, there were almost no identical setups among different reported CRISPR-based methods.

In this work, we proposed and developed a figure of merit (FOM) for CRISPR-based nucleic acid-sensing systems with the goal to quantitatively benchmark different methods and explore the performance improvement strategies. We developed a kinetic model utilizing a single-enzyme framework and then extended it to bulk (multienzyme) systems. The CRISPRbased nucleic acid-sensing FOM, defined as the product of the LOD and CRISPR reaction time, is analytically established by connecting the LOD and reaction time to various reaction setup properties. Using the developed FOM model, we evaluated five strategies to achieve lower LODs with shorter reaction times (i.e., lowering the FOM value). We also compared the improved efficiency of these five strategies. Finally, we benchmarked a total of 57 published works related to CRISPR-based nucleic acid sensing with reaction and performance parameters available. We found that digital CRISPR offers the best (lowest) FOM among various strategies and represents the most promising route toward amplification-free CRISPR-detection methods.

■ ESTABLISHMENT OF THE CRISPR SENSING FOM

Figure 1 presents the common steps for a CRISPR-based nucleic acid-sensing system. We assume that the CRISPR nucleic acid sensing starts with N_0 copies of the targets (DNA or RNA). Normally, a preamplification step could be performed to increase the copy numbers of the targets. For RNA targets, a reverse transcription (RT) step should be performed before or simultaneously with the amplification. Afterward, the cDNA product could be directly utilized in the Cas12 assay 13,41 and should be transcribed back to RNA targets in the Cas13 assay. 9,42 While each different amplification method has its unique kinetics, the number of the amplified targets (N_1) can be related to the initial target quantity N_0 as $N_1 = AN_0$, where A is the amplification ratio.

After this optional preamplification step, the specific binding of nucleic acids to nonactivated Cas proteins (Cas/crRNA binary complex) would activate Cas proteins (Cas/crRNA/ target ternary complex). Upon activation, Cas12 and Cas13 indiscriminately trans-cleavage ssDNA and ssRNA reporters, respectively. Since the trans-cleavage activity is an enzymatic reaction, the CRISPR assay can be modeled as ³⁷

$$E + S \underset{k_{\text{off}}}{\overset{k_{\text{on}}}{\rightleftharpoons}} ES \xrightarrow{k_{\text{cat}}} P + E$$
(1)

where $k_{\rm on}$, $k_{\rm off}$, and $k_{\rm cat}$ are the forward, reverse, and catalytic rates, respectively. E represents the enzyme (activated Cas protein), S is the substrate (intact reporters), ES is the reaction intermediate (enzyme—substrate reporter complex), and P signifies the product (*i.e.*, cleaved reporters).

To capture the speed of product formation, we started from the reaction speed of each individual activated enzyme. Studies

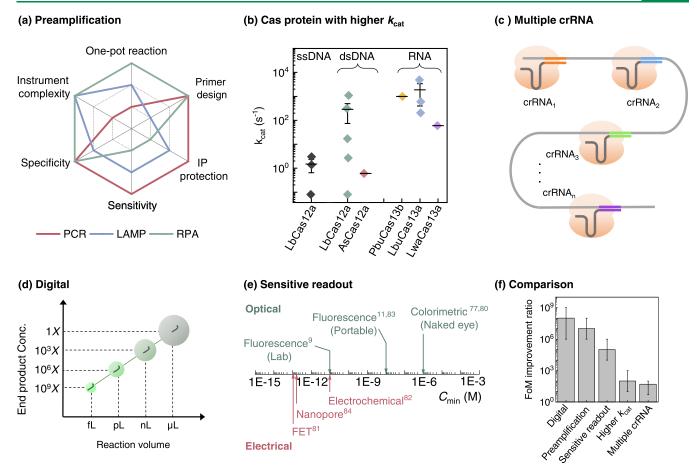


Figure 2. Different strategies to reduce the FOM and improve the CRISPR nucleic acid-sensing performance. (a) Qualitative comparison of three common preamplification methods. (b) Reported catalytic rate constant (k_{cat}) of CRISPR effectors activated by different activators (double- and single-stranded DNAs or RNAs). (c) Schematic of using multiple crRNAs in the CRISPR assay. Introducing n different crRNAs in the assay results in n times more activated Cas in the system and thus increasing the cleavage activity. (d) Effect of digitalization on the product (cleaved reporter) concentration. Reducing the reaction volume effectively increases the signal concentration for a fixed CRISPR reaction time. (e) Comparison of the typical detection limit of various readout methods (C_{min}). (f) Back-of-the-envelope calculation of the FOM improvement ratio using different strategies.

have shown that the single-enzyme reaction is a stochastic process, ⁴⁴ and the reaction speed (s⁻¹) is the reciprocal of the mean waiting time $\langle \tau \rangle$ and can be estimated as follows: $1/\langle \tau \rangle = k_{\rm cat}[S]/(K_{\rm M}+[S])$, where [S] is substrate concentration and $K_{\rm M}$ is Michaelis constant and defined as $(k_{\rm off}+k_{\rm cat})/k_{\rm on}$. Assuming that the total activated enzymes is limited by the number of targets N_1 (i.e., the input Cas/crRNA binary complex is more than the nucleic acid targets, with or without amplification), we can obtain the reaction speed (s⁻¹) for the CRISPR reaction as

$$\nu = N_{\rm l} k_{\rm cat} \frac{[S]}{K_{\rm M} + [S]} \tag{2}$$

With a CRISPR incubation reaction time of T and reaction volume of V_r , the concentration of the cleaved product would be vT/V_r . To effectively detect the cleaved products, the product concentration must be larger than the readout system's limit of detection C_{\min} ($vT/V_r > C_{\min}$). As a result, we can obtain a critical equation for the CRISPR-based nucleic acid sensing

$$N_0 \ge \frac{V_{\rm r}C_{\rm min}}{ATk_{\rm cat}\frac{[S]}{K_{\rm M} + [S]}} \tag{3}$$

This equation means that the lowest quantity of a target concentration (*i.e.*, LOD) that can be detected in a specific CRISPR assay is given by

$$LOD = \frac{\min(N_0)}{V_0} = \frac{V_r C_{\min}}{V_0 A T k_{\text{cat}} \frac{[S]}{K_M + [S]}}$$
(4)

where V_0 is the target sample volume in the Cas reaction. In theory, increasing the V_0 would decrease the LOD of the system. However, V_0 between 1 and 5 μ L has been used in most reported Cas reactions. ^{9,11,18} This is because increasing the V_0 could affect the assay buffer. ¹⁸ From eq 4, we can observe a clear tradeoff between the LOD and CRISPR reaction time (T). To benchmark different CRISPR assays, we defined a figure of merit (FOM) for CRISPR-based nucleic acid sensing as the product of the LOD and reaction time

FOM = LOD ×
$$T = \frac{V_r C_{\min}}{V_0 A k_{\text{cat}} \frac{[S]}{K_M + [S]}}$$
 (5)

This CRISPR-based sensing FOM could be utilized to benchmark the performance of different assays as it is related to experimental conditions such as preamplification (A), the reaction volume (V_r) , readout system (C_{\min}) , and enzymatic

efficiency $(k_{\text{cat}}, K_{\text{M}})$. A smaller FOM value means that lower quantities of the target could be detected faster. It is noteworthy that LOD and reaction time are not equally important for different application scenarios. The FOM presented here should be used as a guide if the test needs to meet certain turnaround times or LOD requirements.

■ FOM IMPROVEMENT STRATEGIES

Use of Preamplification. Based on eq 5, the FOM has a reverse relation with the amplification ratio (A). This implies that utilizing amplification with higher A would decrease the FOM and improve the overall sensing performances. In fact, various preamplification methods such as polymerase chain reaction (PCR), 8,27,45 loop-mediated isothermal amplification (LAMP), \$,16,23 and recombinase polymerase amplification (RPA)^{9,19,46} and their reverse transcriptase (RT) version³⁸ were adopted in CRISPR assays. For example, in the Cas13based SHERLOCK system, RPA was used to improve the LOD of the system up to 6 orders of magnitude. In the Cas12-based HOLMES system, the LOD was improved by 7 orders of magnitude by introducing a 45 min PCR preamplification to the assay.8 However, it is noteworthy that while preamplification could improve the FOM of the CRISPR system significantly, utilizing this additional step complicates the assay design and could increase the cost and assay time. One might be intrigued by the question of why utilizing the CRISPR-based sensing if amplification techniques such as PCR or LAMP could already be used as the testing tools. The answer to this question is that sequence-dependent recognition of target nucleic acids by CRISPR effectors could significantly enhance the specificity and minimize the false positives in the amplification process.

Figure 2a shows a radar chart comparing the six performance metrics of three common preamplification strategies used in CRISPR assays. (1) One-pot reaction. While the preamplification could be performed separately before the CRISPR assay in a two-step reaction, it is preferable to combine the preamplification and the CRISPR assay in a one-pot reaction to simplify the assay setup, decrease the assay time, and reduce the risk of contaminations.³⁴ To this end, the reaction temperature between the preamplification and the CRISPR assay should be compatible. In this regard, RPA is the most suitable preamplification method to couple with CRISPR assays since the reaction temperature is similar $(\sim 37 \, ^{\circ}\text{C})^{35}$ and PCR is incompatible with CRISPR due to its required thermal cycling. LAMP is somewhere in between due to its isothermal nature and had been used in one-pot CRISPR reactions.⁴⁸ Nevertheless, the required 65 °C working temperature is less compatible with that in the CRISPR assay. 49 (2) Primer design. Both PCR and RPA require only two primers. 50 On the other hand, the LAMP requires four to six primers that bind laterally to distinct sites of the DNA target.⁵¹ Moreover, the preamplification primer design is also restricted by the PAM (Cas12-based)^{41,52} and PFS (Cas13-based)⁹ regions in the target. As a result, designing the LAMP primer is more challenging than the PCR and RPA assay. (3) Intellectual property (IP) protection. PCR is one of the first introduced amplification methods, and the foundational patents for PCR expired in March of 2005 in United States and 2006 in Europe.⁵³ Therefore, various companies could offer PCR reagents across the world.⁵⁴ The LAMP assay was patented by Eiken chemical company (EP 1020534 B) from Japan, and this patent was expired in 2019.55 Currently, various companies

such as New England Biolabs and Thermofisher in United States and OptiGene in Europe offer the required reagents for LAMP assay. 56,57 On the other hand, RPA was introduced recently by TwistDx Limited from United Kingdom. 55 So far, only TwistDx and Alere offer RPA reagents.⁵⁸ (4) Sensitivity. The sensitivity of a diagnostic test is defined as the number of true positives (judged by the "Gold Standard") over the total number received a positive result on this test. Li et al. 59 reviewed over 50 studies and compared the sensitivity of RPA with PCR. They showed that the sensitivity of RPA is only half as the PCR. (5) Specificity. The specificity of a diagnostic test is defined as the number of true negatives (judged by the "Gold Standard") over the total number received a negative result on this test. Although the sensitivity of the RPA was not comparable to PCR results, their specificity is comparable.⁵⁹ On the other hand, the complexity of primer design and the number of primers involved in LAMP reaction can lead to false positives from nonspecific primer interactions.⁴⁷ (6) Instrument complexity. To deploy the CRISPR-based diagnosis at the point of care, it is preferred to perform the assay with simple, easy-touse, and cost-effective instruments. 34,35 Both LAMP and RPA are isothermal assays that could be performed using simple equipment ⁶⁰ or even equipment free. ^{61–63} On the other hand, the PCR method relies on thermal cycling, making the instrumentation more complex.

Use of Cas Proteins with Higher k_{cat} . According to eq 5, FOM has a reverse relation with the activated Cas catalytic rate (k_{cat}) . Assuming that all other factors remain the same, Cas proteins with higher $k_{\rm cat}$ would decrease the FOM of the CRISPR system. Different Cas proteins have shown different trans-cleavage activity with various catalytic rates. 21,64-69 Figure 2b presents the k_{cat} of different CRISPR effectors reported by different groups. 21,37,52,64,66-70 It should be noted that these results do not cover all discovered Cas proteins. Further studies are needed to explore the kinetics of various uncharacterized Cas proteins. We observed four interesting features from these data. First, different Cas proteins have distinct k_{cat} . Cas13 effectors generally have a higher cleavage rate. For example, the average $k_{\rm cat}$ of LbuCas13a is around 1861 s⁻¹, much higher than the 279 s⁻¹ for LbCas12a with the dsDNA activator. Second, similar Cas proteins from different bacteria show different cleavage activity, where the average reported k_{cat} for LbCas12a is 2 orders of magnitude larger than that of AsCas12a. Third, different activators would result in different cleavage activities. In the case of Lbcas12a, the average k_{cat} of dsDNA activator cases are around 100 times higher than that of ssDNA activators. Fourth, we observed a significant dispersion between the reported k_{cat} for a specific Cas protein. For instance, the k_{cat} of Lbcas12a with a dsDNA activator ranges from 0.08 to 1089 s⁻¹. This result shows that the combination of identical Cas proteins with different sequences of crRNAs would result in different trans-cleavage speeds. In addition, Nguyen et al.⁶⁴ showed that crRNA extensions could also affect the Cas trans-cleavage activity. Their finding showed that adding a 7-mer ssDNA extension to the 3'-end of crRNA would improve the trans-cleavage activity of LbCas12a proteins (more than 2 times). It should be noted that all of the k_{cat} values presented here are at the optimal temperature for the Cas protein trans-cleavage activity (around 37 °C). 71 We believe that changing the temperature would affect the $k_{\rm cat}$ of the Cas proteins, which alters the system's FOM. The results from Figure 2b suggest that different combinations of Cas proteins, target activators, and crRNAs

should be optimized to obtain the highest $k_{\rm cat}$. From these reported data in Figure 2b, selecting an optimal enzyme could reduce the FOM up to 3 orders of magnitude.

Use of Multiple crRNA in the Reaction. Another strategy to reduce the FOM of CRISPR systems is the use of multiple crRNAs. Combining different crRNAs with Cas proteins would enhance the population of Cas/crRNA binary complex in the same reaction. Consequently, one target would activate multiple Cas proteins in the assay (Figure 2c). Considering that different crRNAs would have different kinetics properties ($K_{\rm M}$ and $k_{\rm cat}$), the reaction speed with multiple crRNA can be written as

$$\nu = N_{1}A \sum_{i=1}^{n} \frac{k_{\text{cat}_{i}}[S]}{K_{M_{i}} + [S]}$$
(6)

where n is the number of crRNAs in the assay. Based on eq 6, increasing the number of crRNA could increase the cleavage rate.

Recent studies have utilized this technique to improve the CRISPR sensing performance. Fozouni et al. used three different crRNAs in developing an amplification-free method for detecting SARS-CoV-2 with CRISPR-Cas13a.⁶⁹ They showed that the LOD was improved 100-fold with the same CRISPR reaction time. In another study, Son et al.⁷² utilized 26 different crRNAs in a Cas13a assay and improved the LOD 5 times. It is clear that utilizing multiple crRNAs could decrease the FOM value and improve the system performance. Nevertheless, the enhancement of the performance using this strategy is additive in nature (eq 6) and is unlikely to offer more than 2 orders of magnitude improvements. In addition, utilizing multiple crRNAs could increase the cost significantly.

Use of Digital CRISPR. The FOM model also suggests that the CRISPR assay performance has a reverse relation with the reaction volume. Decreasing the reaction volume from microliter-scale to sub-nanoliter would improve the FOM of the system. In digital assays, bulk reaction volumes ($\sim \mu L$) are partitioned into thousands or millions of small reaction chambers with pL to fL volumes.⁷³ Figure 2d depicts the effect of reaction volume reduction on the product (cleaved reporter) concentration. As shown, the concentration of the product could increase up to 9 orders of magnitude. A few recent studies have utilized digital CRISPR to improve the performance of the assay. For instance, Tian et al. improved the LOD by 5 orders of magnitude by reducing the reaction volume to 15 pL.74 Besides enhancing the FOM, another advantage of digitalized assays is the ability of absolute target quantification without the need for a standard curve. 65,75,76 Using Poisson statistics, the sample concentration can be estimated by $-\ln(1-p)$, where p is the ratio of the positive partitions over total partitions. Compared to other strategies, digital CRISPR could improve the FOM significantly (more than 6 orders of magnitude).

Use of Sensitive Readout Systems. Another parameter to improve the CRISPR FOM is the readout system's limit of detection C_{\min} . Sensitive readout systems with lower C_{\min} could help achieve lower FOM and better sensing performance (eq 5). While the majority of Cas12 or Cas13-based sensing systems were based on fluorescence signal, 11,16,77 colorimetric, 15,78 electrochemical, 14,21 and electronic readout 45,79 were also explored for signal readout. Figure 2e compares the reported C_{\min} of different readout systems. Among the optical methods, while simple signal readout systems such as

the naked eye and portable fluorescent reader do not offer high sensitivity compared to other methods, they are appealing in developing cost-effective point of care devices. In addition, electrical systems such as the field-effect transistor (FET) biosensors and nanopore sensors offer a lower limit of detection (lower than 1 pM) and the potential for developing an integrated system.

Comparison of FOM Improvement Strategies. Figure 2f summarizes the FOM improvement ratio using these strategies. The improvement ratio was estimated using the FOM model (eq 5) with reported LOD and CRISPR reaction times of previous studies. 8,9,64,69,85,86 As shown, preamplification and digital assays are most effective in improving the FOM. They could significantly improve the FOM by orders of magnitude $(\sim 10^6 - 10^9)$ if used individually. Nevertheless, it should be noted that combining the preamplification and digital assays together would not significantly improve the FOM. This is because the amplified products are not tested in a single reaction volume of V_0 , but rather aliquoted into thousands to millions of smaller chambers. Each of these chambers only has 0 or 1 amplified product (i.e., digital assays). As a result, factors A and V_0 in eq 5 are not multipliable when combining the preamplification and digital methods.

As also shown in Figure 2f, utilizing a sensitive readout system could improve the FOM by 3–5 orders of magnitude compared to a simple readout like using a naked eye. In comparison, utilizing multiple crRNA or different Cas proteins is less effective, although they can still improve the FOM by about 2 orders of magnitude. It is noteworthy that multiple strategies could be implemented in one system to achieve lower FOM compared to individual strategies. For instance, Son et al.⁷² combined digitalization and multiple crRNA in a single system and reduced the FOM by more than 6 orders of magnitude compared to the nonamplified Sherlock system.⁹

To guide the implementation of improvement strategies for different applications, we summarized the advantages and disadvantages of each strategy in Table 1. While preamplifi-

Table 1. Comparisons of Pros and Cons of Different Strategies

| strategy | advantages | disadvantages |
|---|---|--|
| preamplification | high impact on the FOM (more than 6-fold) | longer or multistep assay, higher cost |
| Cas proteins with higher k_{cat} | easy to implement | limited discovered Cas proteins |
| multiple crRNA | easy to implement | low impact on the FOM (less than 2- fold), higher cost |
| digital CRISPR | high impact on the FOM (more than 6-fold), absolute quantification capability | partitioning needed |
| sensitive readout system | medium impact on the FOM (more than 4-fold) | sophisticated instrument, higher cost |

cation, digital assays, and sensitive readout have a high impact on the FOM (more than 4-fold), they would increase the cost and complexity of the systems. On the other hand, utilization of multiple crRNA and Cas proteins with higher $k_{\rm cat}$ is easy to implement in the system; however, they have a lower impact on the FOM (less than 3-fold). One should carefully balance the tradeoff between the cost and the performance when implementing these strategies to meet their testing goals.

Table 2. Summary of the Reported CRISPR-Based Diagnostics with LOD and CRISPR Reaction Time Available

| pathogen | target | effector | readout system | amplification | amplification time (min) | CRISPR reaction time (min) | LOD (aM) | FOM (aM·min) | re |
|-------------------------------|--------|-----------|-----------------|--------------------------|--------------------------|----------------------------|---------------------|-------------------------|----|
| | | | Eı | nsemble without A | Amplification | | | | |
| African swine fever (ASF) | DNA | LbCas12a | fluorescence | none | none | 480 | 1×10^{6} | 4.8×10^{8} | 11 |
| African swine fever | DNA | LbCas12a | fluorescence | none | none | 1440 | 1×10^{5} | 1.4×10^{8} | 11 |
| seudorabies virus | DNA | LbCas12a | fluorescence | none | none | 15 | 1×10^{8} | 1.5×10^{9} | 8 |
| ver cancer | DNA | LbCas12a | colorimetric | none | none | 60 | 2×10^{8} | 1.2×10^{10} | 15 |
| IPV | RNA | LbCas12a | electrochemical | none | none | 60 | 3×10^{7} | 1.8×10^{9} | 10 |
| ika virus | RNA | LwCas13a | fluorescence | none | none | 60 | 5×10^{5} | 3×10^{7} | 9 |
| ARS-CoV-2 | RNA | LbuCas13a | fluorescence | none | none | 120 | 1.6×10^{4} | 1.9×10^{6} | 69 |
| ynthesized target | RNA | LbuCas13a | fluorescence | none | none | 120 | 1×10^{6} | 1.2×10^{8} | 10 |
| ynthesized target | RNA | LbuCas13a | fluorescence | none | none | 20 | 3.7×10^{9} | 7.4×10^{10} | 8 |
| IPV | DNA | LbCas12a | electrochemical | none | none | 60 | 5×10^{7} | 3×10^{9} | 2 |
| niR-19b and miR- 20a | mRNA | LwaCas13a | electrochemical | none | none | 15 | 1×10^7 | 1.5×10^{8} | 14 |
| ENV-4 | DNA | AsCas12a | electrochemical | none | none | 120 | 1×10^{5} | 1.2×10^{7} | 9 |
| BRCA-1 | DNA | AsCas12a | fluorescence | none | none | 30 | 1×10^{3} | 3×10^{4} | 9 |
| HPV | DNA | LbCas12a | fluorescence | none | none | 60 | 1×10^{4} | 6×10^{5} | 92 |
| Bacillus anthracis gene | DNA | LbCas12a | fluorescence | none | none | 15 | 1×10^7 | 1.5×10^{8} | 9 |
| ynthesized target | DNA | LbCas12a | fluorescence | none Ensemble with Ar | none nplification | 60 | 1×10^5 | 6×10^6 | 90 |
| trus greening | DNA | LbCas12a | fluorescence | LAMP | 40 | 5 | 16.6 | 83 | 1 |
| disease frican swine fever | DNA | LbCas12a | fluorescence | LAMP | 40 | 20 | 3.6 | 72 | 1 |
| (ASF) | | | | | | | | | |
| PV | DNA | LbCas12a | fluorescence | RPA | 15 | 60 | 16.6 | 1×10^{3} | 1 |
| SF | DNA | LbCas12a | fluorescence | RPA | 30 | 60 | 10 | 600 | 1 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA | 30 | 30 | 16.6 | 498 | 1 |
| IPV | DNA | LbCas12a | fluorescence | RPA PCR | 10 | 60 | 10 | 600 | 5 |
| seudorabies virus | DNA | LbCas12a | fluorescence | | 45 | 15 | 10 | 150 3.2×10^3 | 8 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA (one pot) | none | 40 | 80.3 | | 2 |
| seudomonas aeruginosa | DNA | LbCas12a | colorimetric | LAMP | 15 | 30 | 3.4 | 102 | 1 |
| IPV | DNA | LbCas12a | colorimetric | PCR | 50 | 30 | 240 | 7.2×10^3 | 1 |
| bola virus | RNA | LbCas12a | fluorescence | RPA | 40 | 240 | 10 | 2.4×10^{3} | 4 |
| nthesized target | RNA | AacCas12b | fluorescence | LAMP | 30 | 30 | 10 | 300 | 1 |
| ARS-CoV-2 | RNA | AacCas12b | fluorescence | RAA | 30 | 30 | 16.6 | 498 | 2 |
| ka virus | RNA | LwCas13a | fluorescence | RPA | 120 | 60 | 2 | 120 | 9 |
| ka virus | RNA | LbuCas13a | fluorescence | RPA | 20 | 60 | 6 | 360 | 1 |
| ytomegalovirus | DNA | LwCas13a | fluorescence | RPA | 50 | 180 | 0.6 | 108 | 1 |
| hite spot syndrome | RNA | Cas13a | colorimetric | RPA | 40 | 180 | 1.6 | 288 | 1 |
| arious tumor cells | mRNA | LbuCas13a | electrochemical | EXPAR | 30 | 30 | 1×10^{3} | 3×10^{4} | 2 |
| ARS-CoV-2 | RNA | AsCas12a | nanopore | PCR | 30 | 30 | 22.5 | 675 | 4 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | LAMP | 30 | 10 | 16.6 | 166 | 2 |
| ARS-CoV-2 | RNA | AsCas12a | fluorescence | LAMP | 30 | 30 | 8.3 | 249 | 2 |
| ARS-CoV-2 | RNA | LwaCas13a | fluorescence | RPA | 20 | 60 | 16.6 | 996 | 2 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | LAMP | 20 | 15 | 16.6 | 249 | 1 |
| IPV | DNA | AaCas12b | fluorescence | RPA | 10 | 180 | 1 | 180 | 1 |
| ARS-CoV-2 | RNA | AapCas12b | fluorescence | LAMP (one pot) | none | 60 | 3.3 | 198 | 4 |
| ifferent viruses | RNA | LwaCas13a | fluorescence | PCR or RPA | 20 | 180 | 0.9 | 162 | 9 |
| ARS-CoV-2 | RNA | LbCas12a | colorimetric | RPA | 30 | 20 | 8.3 | 166 | 9 |
| isteria monocytogenes | DNA | LbCas12a | electrochemical | RAA | 30 | 90 | 0.68 | 61.2 | 9 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA | 30 | 10 | 16.6 | 166 | 9 |
| ARS-CoV-2 | RNA | LwaCas13a | fluorescence | PCR | 22 | 30 | 332 | 1×10^4 | 2 |
| ARS-CoV-2 | RNA | LbCas12a | colorimetric | RPA | 20 | 60 | 1.6 | 96 | 9 |
| ARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA | 15 | 25 | 83 | 2.1×10^{3} | 8 |
| taphylococcus aureus | DNA | LbCas12a | colorimetric | RAA | 20 | 30 | 1 | 30 | 8 |

Table 2. continued

| pathogen | target | effector | readout system | amplification | amplification time (min) | CRISPR reaction time (min) | LOD (aM) | FOM (aM·min) | ref |
|-------------------------------|--------|-----------|----------------|----------------|--------------------------|----------------------------|----------|---------------------|-----|
| SARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA (one pot) | none | 60 | 2 | 120 | 113 |
| SARS-CoV-2 | RNA | LbCas12a | fluorescence | LAMP | 10 | 25 | 6.5 | 162.5 | 114 |
| SARS-CoV-2 | RNA | LbCas12a | fluorescence | LAMP | 40 | 10 | 26 | 260 | 115 |
| Ensemble Using Multiple crRNA | | | | | | | | | |
| SARS-CoV-2 | RNA | LbuCas13a | fluorescence | none | none | 120 | 166 | 2×10^{4} | 69 |
| synthesized target | DNA | LbCas12a | fluorescence | none | none | 30 | 310 | 9.3×10^{3} | 117 |
| Digital without Amplification | | | | | | | | | |
| ASF | DNA | LbCas12a | fluorescence | none | none | 60 | 30 | 1.8×10^{3} | 65 |
| SARS-CoV-2 | RNA | LbuCas13a | fluorescence | none | none | 60 | 10 | 600 | 74 |
| SARS-CoV-2 | RNA | LbuCas13a | fluorescence | none | none | 15 | 8.3 | 124.5 | 72 |
| Digital with Amplification | | | | | | | | | |
| SARS-CoV-2 | RNA | LbCas12a | fluorescence | RPA (one pot) | none | 60 | 1.5 | 90 | 86 |
| SARS-CoV-2 | RNA | Cas12a | fluorescence | RPA (one pot) | none | 60 | 1.6 | 96 | 85 |
| SARS-CoV-2 | RNA | LbCas12a | fluorescence | DAMP (one pot) | none | 50 | 8.3 | 415 | 39 |
| SARS-CoV-2 | RNA | AapCas12b | fluorescence | LAMP (one pot) | none | 120 | 23 | 2.7×10^3 | 118 |
| Digital Using Multiple crRNA | | | | | | | | | |
| SARS-CoV-2 | RNA | LbuCas13a | fluorescence | none | none | 15 | 1.6 | 24 | 72 |

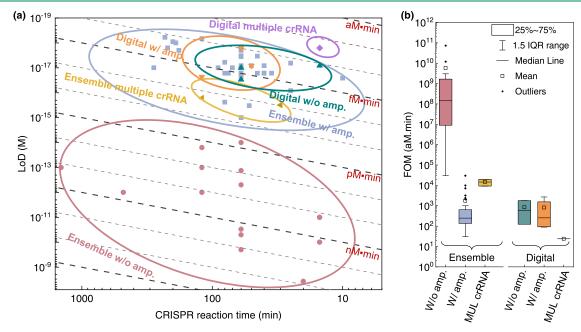


Figure 3. (a) Scattering plot of the limit of detection *versus* CRISPR reaction time for a total of 57 CRISPR-based sensing studies, along with the FOM-equivalent dash lines from 10^{-18} to 10^{-6} M·min. The data points were divided into six categories separated by the ovals in the figure. The top right side of the figure indicates a lower FOM and thus a better CRISPR sensing performance. Within each category, the data points do not perfectly reside on a single line (LOD \times T = constant). This is because the used Cas protein, crRNA, target, amplification method, and readout system could vary within each category. (b) Box graph presents the FOM range of each category. IQR stands for the interquartile range of the FOM data.

■ PERFORMANCE BENCHMARKING

Numerous CRISPR-based nucleic acid-sensing systems were reported in the past several years. 35,40,87 The FOM model described in eq 5 provides us with a tool to benchmark the performance of these different systems. We studied a total of 57 published works (Table 2) related to CRISPR-based nucleic a c i d s e n s i n g u p t o t h i s d a t e (F e b 2022). 8,9,14-16,19-21,23-28,39,45,46,48,52,65,69,72,74,83,85,86,88-118 It is noteworthy that while many more CRISPR-based sensing

studies have been published in the past few years, we only include those with the LOD and CRISPR reaction time available. It should be mentioned that Cas9^{4,6} and Cas14¹¹⁹ have been utilized for diagnostics. However, in this study, we look into Cas12 and Cas13-based systems since they are more common and parameters for comparison are available.

Figure 3a shows the LOD *versus* CRISPR reaction time scattering plots along with the FOM-equivalent dash lines from 10^{-6} to 10^{-18} M·min. Note that the upper-right corner

represents a smaller FOM value and is thus preferred since it means lower LODs can be achieved by shorter CRISPR reaction times. We observed three important features in Figure 3a. First, these data points were divided into six categories based on the strategies they used (shown as oval in Figure 3a): (1) ensemble without amplification, (2) ensemble with amplification, (3) ensemble using multiple crRNA, (4) digital without amplification, (5) digital with amplification, and (6) digital using multiple crRNA. To benchmark these categories, we plotted the FOM values for each category (Figure 3b). As shown, the category of the ensemble without amplification represents the plain vanilla version of the CRISPR-based sensing. The data points within this category show the worst (highest) FOM (with an average of 5.8 × 10¹⁹ aM·min). The data points from all other categories show significant FOM improvements. For example, ensemble with amplification, ensemble using multiple crRNA, digital without amplification, digital with amplification, and digital using multiple crRNA strategies in average improved the FOM by 6, 5, 6, 6, and 8 orders of magnitude, respectively. These improvement results are consistent with the predictions in Figure 2f.

Second, as shown in Figure 3b, FOM in the order of 1–10 fM·min could be achieved within the digitalization categories with or without preamplification. This means that a target concentration of 100 aM to 1 fM could be obtained in 10 min CRISPR reaction time using digital assays without amplification, which was experimentally validated. The best FOM performance was observed by combining digital assay and multiple crRNA cases, where FOM deceased to 24 aM·min. As a result, digital CRISPR assay provides the most appealing method for amplification-free CRISPR-based nucleic acid sensing. Since digital CRISPR-based sensing is a new trend, limited data is available and more studies in the future would improve this evaluation.

Third, we observed a general reverse relation between the LOD and reaction time. Based on eq 4, the logarithmic LOD (log LOD) and logarithmic reaction time (log T) are expected to have a relationship of -1 within each category in which reaction parameters are similar. To test this prediction, we examined the categories of ensemble assays with amplification and ensemble assays without amplification, as both categories have sufficient data points to establish meaningful statistics. A linear fitting revealed the slope in the ensemble assays with and without amplification is -0.9 ± 0.3 and -1.2 ± 0.5 , respectively, consistent with the model predictions (-1).

CONCLUSIONS

In summary, we proposed and developed a figure of merit (FOM) for cleavage-based CRISPR nucleic acid-sensing systems to quantitatively benchmark different methods and explore the performance improvement strategies. The CRISPR-based nucleic acid-sensing FOM, defined as the product of the LOD and CRISPR reaction time, is analytically established by connecting the LOD and reaction time to various reaction setup properties. Based on the developed model, we found that the CRISPR sensing FOM was linked to the reaction volume, the sensitivity of the readout system, preamplification efficiency, and Cas protein enzymatic properties. We evaluated different strategies to reduce the FOM and improve the performance of CRISPR systems, including the use of preamplification, novel Cas proteins with higher k_{cat} multiple crRNA, digital CRISPR, and sensitive readout systems. Comparison of FOM improvement strategies showed that preamplification and digital CRISPR have the highest impact on the FOM (up to 9 orders of magnitude). We benchmarked the FOM performances of 57 existing studies and found that the effectiveness of these strategies on improving the FOM is consistent with the model prediction. In particular, we found that digitalization is the most promising amplification-free method for achieving comparable FOM performances (\sim 1 fM·min) as those using preamplification.

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Author Contributions

W.G. conceived the concept and supervised the study. R.N. developed the FOM model and collected the data for benchmarking the FOM values. R.N., M.D., and A.J.P. analyzed the data. W.G. and R.N. co-wrote the manuscript, with discussion from all authors.

Notes

The authors declare no competing financial interest.

ACKNOWLEDGMENTS

This work was supported by the National Institutes of Health (R61AI147419) and National Science Foundation (1902503, 1912410, 2045169). Any opinions, findings, and conclusions or recommendations expressed in this work are those of the authors and do not necessarily reflect the views of the National Science Foundation and National Institutes of Health.

■ REFERENCES

- (1) Komor, A. C.; Badran, A. H.; Liu, D. R. CRISPR-based technologies for the manipulation of eukaryotic genomes. *Cell* **2017**, *168*, 20–36.
- (2) Pardee, K.; Green, A. A.; Takahashi, M. K.; Braff, D.; Lambert, G.; Lee, J. W.; Ferrante, T.; Ma, D.; Donghia, N.; Fan, M.; et al. Rapid, low-cost detection of Zika virus using programmable biomolecular components. *Cell* **2016**, *165*, 1255–1266.
- (3) Hajian, R.; Balderston, S.; Tran, T.; DeBoer, T.; Etienne, J.; Sandhu, M.; Wauford, N. A.; Chung, J.-Y.; Nokes, J.; Athaiya, M.; et al. Detection of unamplified target genes via CRISPR—Cas9 immobilized on a graphene field-effect transistor. *Nat. Biomed. Eng.* **2019**, *3*, 427–437.

- (4) Zhou, W.; Hu, L.; Ying, L.; Zhao, Z.; Chu, P. K.; Yu, X.-F. A CRISPR—Cas9-triggered strand displacement amplification method for ultrasensitive DNA detection. *Nat. Commun.* **2018**, *9*, No. 5012.
- (5) Quan, J.; Langelier, C.; Kuchta, A.; Batson, J.; Teyssier, N.; Lyden, A.; Caldera, S.; McGeever, A.; Dimitrov, B.; King, R.; et al. FLASH: a next-generation CRISPR diagnostic for multiplexed detection of antimicrobial resistance sequences. *Nucleic Acids Res.* **2019**, *47*, e83.
- (6) Huang, M.; Zhou, X.; Wang, H.; Xing, D. Clustered regularly interspaced short palindromic repeats/Cas9 triggered isothermal amplification for site-specific nucleic acid detection. *Anal. Chem.* **2018**, *90*, 2193–2200.
- (7) Wang, T.; Liu, Y.; Sun, H. H.; Yin, B. C.; Ye, B. C. An RNA-guided Cas9 nickase-based method for universal isothermal DNA amplification. *Angew. Chem.* **2019**, *131*, 5436–5440.
- (8) Li, S.-Y.; Cheng, Q.-X.; Wang, J.-M.; Li, X.-Y.; Zhang, Z.-L.; Gao, S.; Cao, R.-B.; Zhao, G.-P.; Wang, J. CRISPR-Cas12a-assisted nucleic acid detection. *Cell Discovery* **2018**, *4*, No. 20.
- (9) Gootenberg, J. S.; Abudayyeh, O. O.; Lee, J. W.; Essletzbichler, P.; Dy, A. J.; Joung, J.; Verdine, V.; Donghia, N.; Daringer, N. M.; Freije, C. A.; et al. Nucleic acid detection with CRISPR-Cas13a/C2c2. Science 2017, 356, 438–442.
- (10) Harrington, L. B.; Burstein, D.; Chen, J. S.; Paez-Espino, D.; Ma, E.; Witte, I. P.; Cofsky, J. C.; Kyrpides, N. C.; Banfield, J. F.; Doudna, J. A. Programmed DNA destruction by miniature CRISPR-Cas14 enzymes. *Science* **2018**, *362*, 839–842.
- (11) Gootenberg, J. S.; Abudayyeh, O. O.; Kellner, M. J.; Joung, J.; Collins, J. J.; Zhang, F. Multiplexed and portable nucleic acid detection platform with Cas13, Cas12a, and Csm6. *Science* **2018**, *360*, 439–444.
- (12) Abudayyeh, O. O.; Gootenberg, J. S.; Kellner, M. J.; Zhang, F. Nucleic acid detection of plant genes using CRISPR-Cas13. *CRISPR J.* **2019**, *2*, 165–171.
- (13) Li, S.-Y.; Cheng, Q.-X.; Liu, J.-K.; Nie, X.-Q.; Zhao, G.-P.; Wang, J. CRISPR-Cas12a has both cis-and trans-cleavage activities on single-stranded DNA. *Cell Res.* **2018**, 28, 491–493.
- (14) Bruch, R.; Baaske, J.; Chatelle, C.; Meirich, M.; Madlener, S.; Weber, W.; Dincer, C.; Urban, G. A. CRISPR/Cas13a-powered electrochemical microfluidic biosensor for nucleic acid amplification-free miRNA diagnostics. *Adv. Mater.* **2019**, *31*, No. 1905311.
- (15) Shao, N.; Han, X.; Song, Y.; Zhang, P.; Qin, L. CRISPR-Cas12a Coupled with Platinum Nanoreporter for Visual Quantification of SNVs on a Volumetric Bar-Chart Chip. *Anal. Chem.* **2019**, *91*, 12384–12391.
- (16) Li, L.; Li, S.; Wu, N.; Wu, J.; Wang, G.; Zhao, G.; Wang, J. HOLMESv2: a CRISPR-Cas12b-assisted platform for nucleic acid detection and DNA methylation quantitation. *ACS Synth. Biol.* **2019**, 8, 2228–2237.
- (17) Qin, P.; Park, M.; Alfson, K. J.; Tamhankar, M.; Carrion, R.; Patterson, J. L.; Griffiths, A.; He, Q.; Yildiz, A.; Mathies, R.; Du, K. Rapid and fully microfluidic Ebola virus detection with CRISPR-Cas13a. ACS Sens. 2019, 4, 1048–1054.
- (18) Kellner, M. J.; Koob, J. G.; Gootenberg, J. S.; Abudayyeh, O. O.; Zhang, F. SHERLOCK: nucleic acid detection with CRISPR nucleases. *Nat. Protoc.* **2019**, *14*, 2986–3012.
- (19) Myhrvold, C.; Freije, C. A.; Gootenberg, J. S.; Abudayyeh, O. O.; Metsky, H. C.; Durbin, A. F.; Kellner, M. J.; Tan, A. L.; Paul, L. M.; Parham, L. A.; et al. Field-deployable viral diagnostics using CRISPR-Cas13. *Science* **2018**, *360*, 444–448.
- (20) Dai, Y.; Somoza, R. A.; Wang, L.; Welter, J. F.; Li, Y.; Caplan, A. I.; Liu, C. C. Exploring the Trans-Cleavage Activity of CRISPR-Cas12a (cpf1) for the Development of a Universal Electrochemical Biosensor. *Angew. Chem.* **2019**, *131*, 17560–17566.
- (21) Zhou, T.; Huang, R.; Huang, M.; Shen, J.; Shan, Y.; Xing, D. CRISPR/Cas13a powered portable electrochemiluminescence chip for ultrasensitive and specific MiRNA detection. *Adv. Sci.* **2020**, *7*, No. 1903661.
- (22) Udugama, B.; Kadhiresan, P.; Kozlowski, H. N.; Malekjahani, A.; Osborne, M.; Li, V. Y.; Chen, H.; Mubareka, S.; Gubbay, J. B.;

- Chan, W. C. Diagnosing COVID-19: the disease and tools for detection. ACS Nano 2020, 14, 3822-3835.
- (23) Broughton, J. P.; Deng, X.; Yu, G.; Fasching, C. L.; Servellita, V.; Singh, J.; Miao, X.; Streithorst, J. A.; Granados, A.; Sotomayor-Gonzalez, A.; Zorn, K.; Gopez, A.; Hsu, E.; Gu, W.; Miller, S.; Pan, C.-Y.; Guevara, H.; Wadford, D. A.; Chen, J. S.; Chiu, C. Y. CRISPR—Cas12-based detection of SARS-CoV-2. *Nat. Biotechnol.* **2020**, *38*, 870–874.
- (24) Ali, Z.; Aman, R.; Mahas, A.; Rao, G. S.; Tehseen, M.; Marsic, T.; Salunke, R.; Subudhi, A. K.; Hala, S. M.; Hamdan, S. M.; et al. iSCAN: An RT-LAMP-coupled CRISPR-Cas12 module for rapid, sensitive detection of SARS-CoV-2. *Virus Res.* **2020**, 288, No. 198129.
- (25) Ding, X.; Yin, K.; Li, Z.; Lalla, R. V.; Ballesteros, E.; Sfeir, M. M.; Liu, C. Ultrasensitive and visual detection of SARS-CoV-2 using all-in-one dual CRISPR-Cas12a assay. *Nat. Commun.* **2020**, *11*, No. 4711.
- (26) Guo, L.; Sun, X.; Wang, X.; Liang, C.; Jiang, H.; Gao, Q.; Dai, M.; Qu, B.; Fang, S.; Mao, Y.; et al. SARS-CoV-2 detection with CRISPR diagnostics. *Cell Discovery* **2020**, *6*, No. 34.
- (27) Rauch, J. N.; Valois, E.; Solley, S. C.; Braig, F.; Lach, R. S.; Audouard, M.; Ponce-Rojas, J. C.; Costello, M. S.; Baxter, N. J.; Kosik, K. S.; et al. A scalable, easy-to-deploy protocol for Cas13-based detection of SARS-CoV-2 genetic material. *J. Clin. Microbiol.* **2021**, 59, No. e02402-20.
- (28) Arizti-Sanz, J.; Freije, C. A.; Stanton, A. C.; Petros, B. A.; Boehm, C. K.; Siddiqui, S.; Shaw, B. M.; Adams, G.; Kosoko-Thoroddsen, T.-S. F.; Kemball, M. E.; et al. Streamlined inactivation, amplification, and Cas13-based detection of SARS-CoV-2. *Nat. Commun.* 2020, 11, No. 5921.
- (29) Abbott, T. R.; Dhamdhere, G.; Liu, Y.; Lin, X.; Goudy, L.; Zeng, L.; Chemparathy, A.; Chmura, S.; Heaton, N. S.; Debs, R.; et al. Development of CRISPR as an antiviral strategy to combat SARS-CoV-2 and influenza. *Cell* **2020**, *181*, 865.e12–876.e12.
- (30) Wang, R.; Qian, C.; Pang, Y.; Li, M.; Yang, Y.; Ma, H.; Zhao, M.; Qian, F.; Yu, H.; Liu, Z.; et al. opvCRISPR: One-pot visual RT-LAMP-CRISPR platform for SARS-cov-2 detection. *Biosens. Bioelectron.* **2021**, *172*, No. 112766.
- (31) Ning, B.; Yu, T.; Zhang, S.; Huang, Z.; Tian, D.; Lin, Z.; Niu, A.; Golden, N.; Hensley, K.; Threeton, B.; et al. A smartphone-read ultrasensitive and quantitative saliva test for COVID-19. *Sci. Adv.* **2021**, *7*, No. eabe3703.
- (32) Kaminski, M. M.; Abudayyeh, O. O.; Gootenberg, J. S.; Zhang, F.; Collins, J. J. CRISPR-based diagnostics. *Nat. Biomed. Eng.* **2021**, *5*, 643–656
- (33) Wang, X.; Shang, X.; Huang, X. Next-generation pathogen diagnosis with CRISPR/Cas-based detection methods. *Emerging Microbes Infect.* **2020**, *9*, 1682–1691.
- (34) Nouri, R.; Tang, Z.; Dong, M.; Liu, T.; Kshirsagar, A.; Guan, W. CRISPR-based detection of SARS-CoV-2: A review from sample to result. *Biosens. Bioelectron.* **2021**, *178*, No. 113012.
- (35) van Dongen, J. E.; Berendsen, J. T.; Steenbergen, R. D.; Wolthuis, R. M.; Eijkel, J. C.; Segerink, L. I. Point-of-care CRISPR/Cas nucleic acid detection: recent advances, challenges and opportunities. *Biosens. Bioelectron.* **2020**, *166*, No. 112445.
- (36) Wang, M.; Zhang, R.; Li, J. CRISPR/cas systems redefine nucleic acid detection: principles and methods. *Biosens. Bioelectron.* **2020**, *165*, No. 112430.
- (37) Ramachandran, A.; Santiago, J. G. CRISPR Enzyme Kinetics for Molecular Diagnostics. *Anal. Chem.* **2021**, 93, 7456–7464.
- (38) Yan, W. X.; Chong, S.; Zhang, H.; Makarova, K. S.; Koonin, E. V.; Cheng, D. R.; Scott, D. A. Cas13d is a compact RNA-targeting type VI CRISPR effector positively modulated by a WYL-domain-containing accessory protein. *Mol. Cell* **2018**, *70*, 327.e5–339.e5.
- (39) Ding, X.; Yin, K.; Li, Z.; Sfeir, M. M.; Liu, C. Sensitive quantitative detection of SARS-CoV-2 in clinical samples using digital warm-start CRISPR assay. *Biosens. Bioelectron.* **2021**, *184*, No. 113218.
- (40) Lau, A.; Ren, C.; Lee, L. P. Critical review on where CRISPR meets molecular diagnostics. *Prog. Biomed. Eng.* **2020**, *3*, No. 012001.

- (41) Zetsche, B.; Gootenberg, J. S.; Abudayyeh, O. O.; Slaymaker, I. M.; Makarova, K. S.; Essletzbichler, P.; Volz, S. E.; Joung, J.; Van Der Oost, J.; Regev, A.; et al. Cpf1 is a single RNA-guided endonuclease of a class 2 CRISPR-Cas system. *Cell* **2015**, *163*, 759–771.
- (42) Abudayyeh, O. O.; Gootenberg, J. S.; Konermann, S.; Joung, J.; Slaymaker, I. M.; Cox, D. B.; Shmakov, S.; Makarova, K. S.; Semenova, E.; Minakhin, L.; et al. C2c2 is a single-component programmable RNA-guided RNA-targeting CRISPR effector. *Science* **2016**, 353, No. aaf5573.
- (43) Abudayyeh, O. O.; Gootenberg, J. S. CRISPR diagnostics. *Science* **2021**, *372*, 914–915.
- (44) English, B. P.; Min, W.; Van Oijen, A. M.; Lee, K. T.; Luo, G.; Sun, H.; Cherayil, B. J.; Kou, S.; Xie, X. S. Ever-fluctuating single enzyme molecules: Michaelis-Menten equation revisited. *Nat. Chem. Biol.* **2006**, *2*, 87–94.
- (45) Nouri, R.; Jiang, Y.; Tang, Z.; Lian, X. L.; Guan, W. Detection of SARS-CoV-2 with Solid-State CRISPR-Cas12a-Assisted Nanopores. *Nano Lett.* **2021**, *21*, 8393–8400.
- (46) English, M. A.; Soenksen, L. R.; Gayet, R. V.; de Puig, H.; Angenent-Mari, N. M.; Mao, A. S.; Nguyen, P. Q.; Collins, J. J. Programmable CRISPR-responsive smart materials. *Science* **2019**, 365, 780–785.
- (47) Hardinge, P.; Murray, J. A. Lack of specificity associated with using molecular beacons in loop mediated amplification assays. *BMC Biotechnol.* **2019**, *19*, No. 55.
- (48) Joung, J.; Ladha, A.; Saito, M.; Kim, N.-G.; Woolley, A. E.; Segel, M.; Barretto, R. P.; Ranu, A.; Macrae, R. K.; Faure, G.; et al. Detection of SARS-CoV-2 with SHERLOCK one-pot testing. *N. Engl. J. Med.* **2020**, 383, 1492–1494.
- (49) Thi, V. L. D.; Herbst, K.; Boerner, K.; Meurer, M.; Kremer, L. P.; Kirrmaier, D.; Freistaedter, A.; Papagiannidis, D.; Galmozzi, C.; Stanifer, M. L.; Boulant, S.; Klein, S.; Chlanda, P.; Khalid, D.; Miranda, I. B.; Schnitzler, P.; Kräusslich, H.-G.; Knop, M.; Anders, S. A colorimetric RT-LAMP assay and LAMP-sequencing for detecting SARS-CoV-2 RNA in clinical samples. *Sci. Transl. Med.* **2020**, *12*, No. eabc7075.
- (50) Higgins, M.; Ravenhall, M.; Ward, D.; Phelan, J.; Ibrahim, A.; Forrest, M. S.; Clark, T. G.; Campino, S. PrimedRPA: Primer design for recombinase polymerase amplification assays. *Bioinformatics* **2019**, 35, 682–684.
- (51) Tomita, N.; Mori, Y.; Kanda, H.; Notomi, T. Loop-mediated isothermal amplification (LAMP) of gene sequences and simple visual detection of products. *Nat. Protoc.* **2008**, *3*, 877–882.
- (52) Chen, J. S.; Ma, E.; Harrington, L. B.; Da Costa, M.; Tian, X.; Palefsky, J. M.; Doudna, J. A. CRISPR-Cas12a target binding unleashes indiscriminate single-stranded DNase activity. *Science* **2018**, *360*, 436–439.
- (53) McDowell, D. The polymerase chain reaction patents: going, going,... still going. J. R. Soc. Med. **2006**, 99, 62–64.
- (54) Bezier, C.; Anthoine, G.; Charki, A. Reliability of real-time RT-PCR tests to detect SARS-Cov-2: A literature review. *Int. J. Metrol. Qual. Eng.* **2020**, *11*, No. 13.
- (55) Obande, G. A.; Singh, K. K. B. Current and future perspectives on isothermal nucleic acid amplification technologies for diagnosing infections. *Infect. Drug Resist.* **2020**, 455.
- (56) Keizerweerd, A. T.; Chandra, A.; Grisham, M. P. Development of a reverse transcription loop-mediated isothermal amplification (RT-LAMP) assay for the detection of Sugarcane mosaic virus and Sorghum mosaic virus in sugarcane. *J. Virol. Methods* **2015**, *212*, 23–29
- (57) Huang, W. E.; Lim, B.; Hsu, C. C.; Xiong, D.; Wu, W.; Yu, Y.; Jia, H.; Wang, Y.; Zeng, Y.; Ji, M.; et al. RT-LAMP for rapid diagnosis of coronavirus SARS-CoV-2. *Microb. Biotechnol.* **2020**, *13*, 950–961.
- (58) Li, J.-j.; Xiong, C.; Liu, Y.; Liang, J.-s.; Zhou, X.-w. Loop-mediated isothermal amplification (LAMP): emergence as an alternative technology for herbal medicine identification. *Front. Plant Sci.* **2016**, *7*, No. 1956.

- (59) Li, J.; Macdonald, J.; von Stetten, F. a comprehensive summary of a decade development of the recombinase polymerase amplification. *Analyst* **2019**, *144*, 31–67.
- (60) Lee, S.; Khoo, V. S. L.; Medriano, C. A. D.; Lee, T.; Park, S.-Y.; Bae, S. Rapid and in-situ detection of fecal indicator bacteria in water using simple DNA extraction and portable loop-mediated isothermal amplification (LAMP) PCR methods. *Water Res.* **2019**, *160*, 371–379.
- (61) Wu, Y.-D.; Zhou, D.-H.; Zhang, L.-X.; Zheng, W.-B.; Ma, J.-G.; Wang, M.; Zhu, X.-Q.; Xu, M.-J. Recombinase polymerase amplification (RPA) combined with lateral flow (LF) strip for equipment-free detection of Cryptosporidium spp. oocysts in dairy cattle feces. *Parasitol. Res.* **2016**, *115*, 3551–3555.
- (62) Liu, L.; Wang, J.; Zhang, R.; Lin, M.; Shi, R.; Han, Q.; Wang, J.; Yuan, W. Visual and equipment-free reverse transcription recombinase polymerase amplification method for rapid detection of foot-and-mouth disease virus. *BMC Vet. Res.* **2018**, *14*, No. 263.
- (63) Liu, L.; Wang, J.; Geng, Y.; Wang, J.; Li, R.; Shi, R.; Yuan, W. Equipment-free recombinase polymerase amplification assay using body heat for visual and rapid point-of-need detection of canine parvovirus 2. *Mol. Cell. Probes* **2018**, *39*, 41–46.
- (64) Nguyen, L. T.; Smith, B. M.; Jain, P. K. Enhancement of transcleavage activity of Cas12a with engineered crRNA enables amplified nucleic acid detection. *Nat. Commun.* **2020**, *11*, No. 4906.
- (65) Yue, H.; Shu, B.; Tian, T.; Xiong, E.; Huang, M.; Zhu, D.; Sun, J.; Liu, Q.; Wang, S.; Li, Y.; Zhou, X. Droplet Cas12a Assay Enables DNA Quantification from Unamplified Samples at the Single-Molecule Level. *Nano Lett.* **2021**, *21*, 4643–4653.
- (66) Cofsky, J. C.; Karandur, D.; Huang, C. J.; Witte, I. P.; Kuriyan, J.; Doudna, J. A. CRISPR-Cas12a exploits R-loop asymmetry to form double-strand breaks. *eLife* **2020**, *9*, No. e55143.
- (67) Slaymaker, I. M.; Mesa, P.; Kellner, M. J.; Kannan, S.; Brignole, E.; Koob, J.; Feliciano, P. R.; Stella, S.; Abudayyeh, O. O.; Gootenberg, J. S.; et al. High-resolution structure of Cas13b and biochemical characterization of RNA targeting and cleavage. *Cell Rep.* **2019**, *26*, 3741.e5–3751.e5.
- (68) Shan, Y.; Zhou, X.; Huang, R.; Xing, D. High-fidelity and rapid quantification of miRNA combining crRNA programmability and CRISPR/Cas13a trans-cleavage activity. *Anal. Chem.* **2019**, 91, 5278–5285.
- (69) Fozouni, P.; Son, S.; de León Derby, M. D.; Knott, G. J.; Gray, C. N.; D'Ambrosio, M. V.; Zhao, C.; Switz, N. A.; Kumar, G. R.; Stephens, S. I.; et al. Amplification-free detection of SARS-CoV-2 with CRISPR-Cas13a and mobile phone microscopy. *Cell* **2021**, *184*, 323.e9—333.e9.
- (70) Yu, T.; Zhang, S.; Matei, R.; Marx, W.; Beisel, C. L.; Wei, Q. Coupling smartphone and CRISPR-Cas12a for digital and multiplexed nucleic acid detection. *AIChE J.* **2021**, *67*, No. e17365.
- (71) Kanitchinda, S.; Srisala, J.; Suebsing, R.; Prachumwat, A.; Chaijarasphong, T. CRISPR-Cas fluorescent cleavage assay coupled with recombinase polymerase amplification for sensitive and specific detection of Enterocytozoon hepatopenaei. *Biotechnol. Rep.* **2020**, 27, No. e00485.
- (72) Son, S.; Lyden, A.; Shu, J.; Stephens, S. I.; Fozouni, P.; Knott, G. J.; Smock, D. C.; Liu, T. Y.; Boehm, D.; Simoneau, C.; et al. Sensitive and multiplexed RNA detection with Cas13 droplets and kinetic barcoding. *medRxiv* **2021**, *184*, No. 2021.08.02.21261509.
- (73) Guan, W.; Chen, L.; Rane, T. D.; Wang, T.-H. Droplet digital enzyme-linked oligonucleotide hybridization assay for absolute RNA quantification. *Sci. Rep.* **2015**, *5*, No. 13795.
- (74) Tian, T.; Shu, B.; Jiang, Y.; Ye, M.; Liu, L.; Guo, Z.; Han, Z.; Wang, Z.; Zhou, X. An ultralocalized Cas13a assay enables universal and nucleic acid amplification-free single-molecule RNA diagnostics. *ACS Nano* **2021**, *15*, 1167–1178.
- (75) Hall Sedlak, R.; Jerome, K. R. The potential advantages of digital PCR for clinical virology diagnostics. *Expert Rev. Mol. Diagn.* **2014**, *14*, 501–507.
- (76) Kuypers, J.; Jerome, K. R. Applications of digital PCR for clinical microbiology. *J. Clin. Microbiol.* **2017**, *55*, 1621–1628.

- (77) Wang, B.; Wang, R.; Wang, D.; Wu, J.; Li, J.; Wang, J.; Liu, H.; Wang, Y. Cas12aVDet: a CRISPR/Cas12a-based platform for rapid and visual nucleic acid detection. *Anal. Chem.* **2019**, *91*, 12156–12161.
- (78) Yuan, C.; Tian, T.; Sun, J.; Hu, M.; Wang, X.; Xiong, E.; Cheng, M.; Bao, Y.; Lin, W.; Jiang, J.; et al. Universal and Naked-Eye Gene Detection Platform Based on the Clustered Regularly Interspaced Short Palindromic Repeats/Cas12a/13a System. *Anal. Chem.* **2020**, 92, 4029–4037.
- (79) Nouri, R.; Jiang, Y.; Lian, X. L.; Guan, W. Sequence-Specific Recognition of HIV-1 DNA with Solid-State CRISPR-Cas12a-Assisted Nanopores (SCAN). ACS Sens. 2020, 5, 1273–1280.
- (80) Jazayeri, M. H.; Aghaie, T.; Avan, A.; Vatankhah, A.; Ghaffari, M. R. S. Colorimetric detection based on gold nano particles (GNPs): An easy, fast, inexpensive, low-cost and short time method in detection of analytes (protein, DNA, and ion). Sens. Bio-sens. Res. 2018, 20, 1–8.
- (81) Syu, Y.-C.; Hsu, W.-E.; Lin, C.-T. Review—Field-effect transistor biosensing: Devices and clinical applications. *ECS J. Solid State Sci. Technol.* **2018**, *7*, Q3196.
- (82) Goud, K. Y.; Reddy, K. K.; Khorshed, A.; Kumar, V. S.; Mishra, R. K.; Oraby, M.; Ibrahim, A. H.; Kim, H.; Gobi, K. V. Electrochemical diagnostics of infectious viral diseases: trends and challenges. *Biosens. Bioelectron.* **2021**, *180*, No. 113112.
- (83) Katzmeier, F.; Aufinger, L.; Dupin, A.; Quintero, J.; Lenz, M.; Bauer, L.; Klumpe, S.; Sherpa, D.; Dürr, B.; Honemann, M.; et al. A low-cost fluorescence reader for in vitro transcription and nucleic acid detection with Cas13a. *PLoS One* **2019**, *14*, No. e0220091.
- (84) Zhang, L.; Zhang, K.; Liu, G.; Liu, M.; Liu, Y.; Li, J. Label-free nanopore proximity bioassay for platelet-derived growth factor detection. *Anal. Chem.* **2015**, *87*, 5677–5682.
- (85) Park, J. S.; Hsieh, K.; Chen, L.; Kaushik, A.; Trick, A. Y.; Wang, T. H. Digital CRISPR/Cas-Assisted Assay for Rapid and Sensitive Detection of SARS-CoV-2. *Adv. Sci.* **2021**, *8*, No. 2003564.
- (86) Wu, X.; Tay, J. K.; Goh, C. K.; Chan, C.; Lee, Y. H.; Springs, S. L.; Wang, D. Y.; Loh, K. S.; Lu, T. K.; Yu, H. Digital CRISPR-based method for the rapid detection and absolute quantification of nucleic acids. *Biomaterials* **2021**, *274*, No. 120876.
- (87) Ravi, N.; Cortade, D. L.; Ng, E.; Wang, S. X. Diagnostics for SARS-CoV-2 detection: A comprehensive review of the FDA-EUA COVID-19 testing landscape. *Biosens. Bioelectron.* **2020**, *165*, No. 112454.
- (88) Qian, J.; Huang, D.; Ni, D.; Zhao, J.; Shi, Z.; Fang, M.; Xu, Z. A portable CRISPR Cas12a based lateral flow platform for sensitive detection of *Staphylococcus aureus* with double insurance. *Food Control* **2022**, *132*, No. 108485.
- (89) Yin, K.; Ding, X.; Li, Z.; Sfeir, M. M.; Ballesteros, E.; Liu, C. Autonomous lab-on-paper for multiplexed, CRISPR-based diagnostics of SARS-CoV-2. *Lab Chip* **2021**, *21*, 2730–2737.
- (90) Cheng, X.; Yan, Y.; Chen, X.; Duan, J.; Zhang, D.; Yang, T.; Gou, X.; Zhao, M.; Ding, S.; Cheng, W. CRISPR/Cas12a-Modulated fluorescence resonance energy transfer with nanomaterials for nucleic acid sensing. *Sens. Actuators, B* **2021**, *331*, No. 129458.
- (91) Bogers, J. F.; Berghuis, N. F.; Busker, R. W.; van Booma, A.; Paauw, A.; van Leeuwen, H. C. Bright fluorescent nucleic acid detection with CRISPR-Cas12a and poly (thymine) templated copper nanoparticles. *Biol. Methods Protoc.* **2021**, *6*, No. bpaa020.
- (92) Fu, X.; Shi, Y.; Peng, F.; Zhou, M.; Yin, Y.; Tan, Y.; Chen, M.; Yin, X.; Ke, G.; Zhang, X.-B. Exploring the trans-cleavage activity of CRISPR/Cas12a on gold nanoparticles for stable and sensitive biosensing. *Anal. Chem.* **2021**, *93*, 4967–4974.
- (93) Choi, J.-H.; Lim, J.; Shin, M.; Paek, S.-H.; Choi, J.-W. CRISPR-Cas12a-based nucleic acid amplification-free DNA biosensor via Au nanoparticle-assisted metal-enhanced fluorescence and colorimetric analysis. *Nano Lett.* **2021**, *21*, 693–699.
- (94) Lee, Y.; Choi, J.; Han, H.-K.; Park, S.; Park, S. Y.; Park, C.; Baek, C.; Lee, T.; Min, J. Fabrication of ultrasensitive electrochemical biosensor for dengue fever viral RNA Based on CRISPR/Cpf1 reaction. *Sens. Actuators, B* **2021**, 326, No. 128677.

- (95) Zhang, W. S.; Pan, J.; Li, F.; Zhu, M.; Xu, M.; Zhu, H.; Yu, Y.; Su, G. Reverse Transcription Recombinase Polymerase Amplification Coupled with CRISPR-Cas12a for Facile and Highly Sensitive Colorimetric SARS-CoV-2 Detection. *Anal. Chem.* **2021**, *93*, 4126–4133
- (96) Meng, Q.; Wang, X.; Wang, Y.; Dang, L.; Liu, X.; Ma, X.; Chi, T.; Wang, X.; Zhao, Q.; Yang, G.; et al. Detection of the SARS-CoV-2 D614G mutation using engineered Cas12a guide RNA. *Biotechnol. J.* **2021**, *16*, No. 2100040.
- (97) Li, F.; Ye, Q.; Chen, M.; Zhou, B.; Zhang, J.; Pang, R.; Xue, L.; Wang, J.; Zeng, H.; Wu, S.; et al. An ultrasensitive CRISPR/Cas12a based electrochemical biosensor for *Listeria monocytogenes* detection. *Biosens. Bioelectron.* **2021**, *179*, No. 113073.
- (98) Jiang, Y.; Hu, M.; Liu, A.-A.; Lin, Y.; Liu, L.; Yu, B.; Zhou, X.; Pang, D.-W. Detection of SARS-CoV-2 by CRISPR/Cas12a-Enhanced Colorimetry. ACS Sens. 2021, 6, 1086–1093.
- (99) Ackerman, C. M.; Myhrvold, C.; Thakku, S. G.; Freije, C. A.; Metsky, H. C.; Yang, D. K.; Simon, H. Y.; Boehm, C. K.; Kosoko-Thoroddsen, T.-S. F.; Kehe, J.; et al. Massively multiplexed nucleic acid detection with Cas13. *Nature* **2020**, 582, 277–282.
- (100) Teng, F.; Guo, L.; Cui, T.; Wang, X.-G.; Xu, K.; Gao, Q.; Zhou, Q.; Li, W. CDetection: CRISPR-Cas12b-based DNA detection with sub-attomolar sensitivity and single-base specificity. *Genome Biol.* **2019**, 20, No. 132.
- (101) Ramachandran, A.; Huyke, D. A.; Sharma, E.; Sahoo, M. K.; Huang, C.; Banaei, N.; Pinsky, B. A.; Santiago, J. G. Electric field-driven microfluidics for rapid CRISPR-based diagnostics and its application to detection of SARS-CoV-2. *Proc. Natl. Acad. Sci. U.S.A.* **2020**, *117*, 29518–29525.
- (102) Sullivan, T. J.; Dhar, A. K.; Cruz-Flores, R.; Bodnar, A. G. Rapid, CRISPR-based, field-deployable detection of white spot syndrome virus in shrimp. *Sci. Rep.* **2019**, *9*, No. 19702.
- (103) Kaminski, M. M.; Alcantar, M. A.; Lape, I. T.; Greensmith, R.; Huske, A. C.; Valeri, J. A.; Marty, F. M.; Klämbt, V.; Azzi, J.; Akalin, E.; et al. A CRISPR-based assay for the detection of opportunistic infections post-transplantation and for the monitoring of transplant rejection. *Nat. Biomed. Eng.* **2020**, *4*, 601–609.
- (104) East-Seletsky, A.; O'Connell, M. R.; Knight, S. C.; Burstein, D.; Cate, J. H.; Tjian, R.; Doudna, J. A. Two distinct RNase activities of CRISPR-C2c2 enable guide-RNA processing and RNA detection. *Nature* **2016**, *538*, 270–273.
- (105) Zhang, D.; Yan, Y.; Que, H.; Yang, T.; Cheng, X.; Ding, S.; Zhang, X.; Cheng, W. CRISPR/Cas12a-Mediated interfacial cleaving of hairpin DNA reporter for electrochemical nucleic acid sensing. *ACS Sens.* **2020**, *5*, 557–562.
- (106) Tsou, J.-H.; Leng, Q.; Jiang, F. A CRISPR test for detection of circulating nuclei acids. *Transl. Oncol.* **2019**, *12*, 1566–1573.
- (107) Mukama, O.; Wu, J.; Li, Z.; Liang, Q.; Yi, Z.; Lu, X.; Liu, Y.; Liu, Y.; Hussain, M.; Makafe, G. G.; et al. An ultrasensitive and specific point-of-care CRISPR/Cas12 based lateral flow biosensor for the rapid detection of nucleic acids. *Biosens. Bioelectron.* **2020**, *159*, No. 112143.
- (108) Bai, J.; Lin, H.; Li, H.; Zhou, Y.; Liu, J.; Zhong, G.; Wu, L.; Jiang, W.; Du, H.; Yang, J.; et al. Cas12a-based on-site and rapid nucleic acid detection of African swine fever. *Front. Microbiol.* **2019**, 10, No. 2830.
- (109) Yin, K.; Ding, X.; Li, Z.; Zhao, H.; Cooper, K.; Liu, C. Dynamic aqueous multiphase reaction system for one-pot CRISPR-Cas12a-based ultrasensitive and quantitative molecular diagnosis. *Anal. Chem.* **2020**, *92*, 8561–8568.
- (110) He, Q.; Yu, D.; Bao, M.; Korensky, G.; Chen, J.; Shin, M.; Kim, J.; Park, M.; Qin, P.; Du, K. High-throughput and all-solution phase African Swine Fever Virus (ASFV) detection using CRISPR-Cas12a and fluorescence based point-of-care system. *Biosens. Bioelectron.* **2020**, *154*, No. 112068.
- (111) Qian, C.; Wu, H.; Shi, Y.; Wu, J.; Chen, H. Dehydrated CRISPR-mediated DNA analysis for visualized animal-borne virus sensing in the unprocessed blood sample. *Sens. Actuators, B* **2020**, 305, No. 127440.

- (112) Qian, C.; Wang, R.; Wu, H.; Zhang, F.; Wu, J.; Wang, L. Uracil-mediated new photospacer-adjacent motif of Cas12a to realize visualized DNA detection at the single-copy level free from contamination. *Anal. Chem.* **2019**, *91*, 11362–11366.
- (113) de Puig, H.; Lee, R. A.; Najjar, D.; Tan, X.; Soenksen, L. R.; Angenent-Mari, N. M.; Donghia, N. M.; Weckman, N. E.; Ory, A.; Ng, C. F.; et al. Minimally instrumented SHERLOCK (miSHERLOCK) for CRISPR-based point-of-care diagnosis of SARS-CoV-2 and emerging variants. *Sci. Adv.* **2021**, *7*, No. eabh2944.
- (114) Zhang, Y.; Chen, M.; Liu, C.; Chen, J.; Luo, X.; Xue, Y.; Liang, Q.; Zhou, L.; Tao, Y.; Li, M.; et al. Sensitive and rapid on-site detection of SARS-CoV-2 using a gold nanoparticle-based high-throughput platform coupled with CRISPR/Cas12-assisted RT-LAMP. Sens. Actuators, B 2021, 345, No. 130411.
- (115) Garcia-Venzor, A.; Rueda-Zarazua, B.; Marquez-Garcia, E.; Maldonado, V.; Moncada-Morales, A.; Olivera, H.; Lopez, I.; Zuñiga, J.; Melendez-Zajgla, J. SARS-CoV-2 Direct Detection Without RNA Isolation With Loop-Mediated Isothermal Amplification (LAMP) and CRISPR-Cas12. Front. Med. 2021, 8, No. 627679.
- (116) Lucia, C.; Federico, P.-B.; Alejandra, G. C. An ultrasensitive, rapid, and portable coronavirus SARS-CoV-2 sequence detection method based on CRISPR-Cas12. *BioRxiv* **2020**, 4, No. 2020.02.29.971127.
- (117) Nalefski, E. A.; Patel, N.; Leung, P. J.; Islam, Z.; Kooistra, R. M.; Parikh, I.; Marion, E.; Knott, G. J.; Doudna, J. A.; Le Ny, A.-L. M.; Madan, D. Kinetic analysis of Cas12a and Cas13a RNA-Guided nucleases for development of improved CRISPR-Based diagnostics. *Iscience* 2021, 24, No. 102996.
- (118) Luo, X.; Xue, Y.; Ju, E.; Tao, Y.; Li, M.; Zhou, L.; Yang, C.; Zhou, J.; Wang, J. Digital CRISPR/Cas12b-based platform enabled absolute quantification of viral RNA. *Anal. Chim. Acta* **2022**, *1192*, No. 339336.
- (119) Aquino-Jarquin, G. CRISPR-Cas14 is now part of the artillery for gene editing and molecular diagnostic. *Nanomedicine* **2019**, *18*, 428–431.