Microtubule binding kinetics of membrane-bound kinesin-1 predicts high motor copy numbers on intracellular cargo

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Bidirectional vesicle transport along microtubules is necessary for cell viability and function, particularly in neurons. When multiple motors are attached to a vesicle, the distance a vesicle travels before dissociating is determined by the race between detachment of the bound motors and attachment of the unbound motors. Motor detachment rate constants (k\(_{\text{off}}\)) can be measured via single-molecule experiments, but motor reattachment rate constants (k\(_{\text{on}}\)) are generally unknown, as they involve diffusion through the bilayer, geometrical considerations of the motor tether length, and the intrinsic microtubule binding rate of the motor. To understand the attachment dynamics of motors bound to fluid lipid bilayers, we quantified the microtubule accumulation rate of fluorescently labeled kinesin-1 motors in a 2-dimensional (2D) system where motors were linked to a supported lipid bilayer. From the first-order accumulation rate at varying motor densities, we extrapolated a k\(_{\text{on}}\) that matched single-molecule measurements and measured a 2D k\(_{\text{off}}\) for membrane-bound kinesin-1 motors binding to the microtubule. This k\(_{\text{on}}\) is consistent with kinesin-1 being able to reach roughly 20 tubulin subunits when attaching to a microtubule. By incorporating cholesterol to reduce membrane diffusivity, we demonstrate that this k\(_{\text{on}}\) is not limited by the motor diffusion rate, but instead is determined by the intrinsic motor binding rate. For intracellular vesicle trafficking, this 2D k\(_{\text{on}}\) predicts that long-range transport of 100-nm-diameter vesicles requires 35 kinesin-1 motors, suggesting that teamwork between different motor classes and motor clustering may play significant roles in long-range vesicle transport.

Significance

Long-distance transport of membrane-coated vesicles involves coordination of multiple motors such that at least one motor is bound to the microtubule at all times. Microtubule attachment of a membrane-bound motor comprises 2 steps: diffusing through the lipid bilayer to a binding zone near the microtubule, followed by binding. Using a 2-dimensional (2D) supported lipid bilayer system, we show that membrane diffusion is not the limiting factor for motor attachment. This result suggests that in cells kinesin-1 binding kinetics is not altered by the membrane composition of vesicle cargo. The intrinsically slow binding properties of kinesin-1 suggest that divergent motor binding kinetics and motor clustering regulate long-range vesicle transport.

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vesicle transport is achieved are not well understood. The average travel distance of a vesicle depends on the average number of engaged motors, which in turn is determined by a race between motor attachment and detachment rates (Fig. 1A). Motor detachment is described by the first-order unbinding rate constant \( k_{\text{off}} \), which can be experimentally determined by dividing the single-molecule velocity by the run length (12–14). Measuring the motor attachment rate constant is more complicated because it involves 2 processes—diffusion of motors to a zone in which they are able to bind to the MT (described as a rate constant \( k_{\text{diffusion}} \) into a binding zone with area \( A_{\text{zone}} \), followed by MT binding, described by the first-order binding rate constant, \( k_{\text{attach}} \)). Of these 3 parameters, \( k_{\text{attach}} \) for kinesin-1 has been measured in previous studies (10, 12), and bounds can be put on \( k_{\text{diffusion}} \) based on the diffusion constant of motors in the bilayer. In contrast, the area of the zone in which motors can bind to the MT is less well constrained, although the motor’s contour length provides an upper limit. How these parameters interact and whether cells modulate any or all of these parameters to regulate the speed and directionality of bidirectional transport are not understood. For instance, because different intracellular cargos have different lipid compositions (15–17), it is possible that the different diffusion constants alter motor binding kinetics and thus vesicle transport dynamics. This idea has not been experimentally tested, however.

To better understand the principles that govern cargo transport by vesicle-bound motors, we used a 2-dimensional (2D) lipid bilayer system to approximate the local membrane environment where motors attach to a MT (Fig. 1B). By measuring the rate constant of accumulation of membrane-bound kinesin-1 on MTs, we obtained a 2D bimolecular rate constant for motor attachment and detachment rates (Fig. 1A). We compared this motor accumulation rate constant, \( k_{\text{acc}} \), across different motor densities, and found that \( k_{\text{acc}} \) scaled linearly with motor density on the membrane (Movie S1; Fig. 2 A and C, blue and green curves; and Fig. 2D, blue curve). \( k_{\text{acc}} \) varied from 0.70 ± 0.03 s\(^{-1}\) (mean ± SEM; \( n = 3 \)) at low motor density (\( \sim 4\) motors/\( \mu \)m\(^2\)) up to 1.61 ± 0.12 s\(^{-1}\) (mean ± SEM; \( n = 35 \)) at the highest motor density (\( \sim 250\) motors/\( \mu \)m\(^2\)).

To understand \( k_{\text{acc}} \) in terms of motor binding and unbinding rate constants, we applied a simple kinetic model of membrane-bound kinesin motors (Kin) binding to the surface-bound MT, as follows:

\[
\text{Kin} + \text{MT} \xrightleftharpoons{K_{\text{on}}}{k_{\text{off}}} \text{Kin} \cdot \text{MT}. \tag{1}
\]

Here, \( k_{\text{on}} \) is the 2D bimolecular association rate constant, and \( k_{\text{off}} \) is the first-order motor dissociation rate constant. This
system is identical to a reversible bimolecular interaction in solution (18), with the difference that instead of units of molar$^{-1}$

-second$^{-1}$, $k_{on}^{2D}$ has units of (motors/micrometer)$^{-2}$-second$^{-1}$. It can be shown (see SI Appendix, Supplementary Information Text, for details on derivation) that:

$$k_{acc} = k_{on}^{2D} \cdot [\text{Kin}]_{tot} + k_{off},$$

where [Kin]$_{tot}$ is the surface density of kinesin-1. Thus, for the curves in Fig. 2D, a linear regression of $k_{acc}$ as a function of motor density yields a line with a slope equal to the bimolecular association rate constant, $k_{on}^{2D}$, and a $y$-intercept equal to the first-order motor unbinding rate constant, $k_{off}$. The fitted $k_{off}$ of $0.83 \pm 0.21$ s$^{-1}$ (mean $\pm$ 95% confidence bound of fit) was in good agreement with previous single-molecule measurements for these motors in saturating ATP, where $k_{off}$ = velocity/run length (14, 19). From the linear fit, $k_{on}^{2D}$ in saturating ATP was 0.0034 ± 0.0022 (motor/micrometer)$^{-1}$-s$^{-1}$ (mean $\pm$ 95% confidence bound of fit).

One prediction of this model is that, if we change the $k_{off}$ without changing the $k_{on}^{2D}$, then the slope should be unaffected, and only the $y$-intercept should change. To test this prediction, we measured $k_{acc}$ in the presence of 2 mM adenosine-5’-[(β,γ]-imido) triphosphate (AMPPNP) (Movie S1 and Fig. 2 B and C, red and magenta curves), instead of ATP. This nonhydrolyzable ATP analog prevents kinesin-1 dissociation from MT, thus reducing $k_{off}$ to 0 s$^{-1}$. As shown in the red curve in Fig. 2D, $k_{acc}$ scaled linearly with motor density in AMPPNP, and $k_{off}$ was near zero (0.10 ± 0.07 s$^{-1}$), as expected. The $k_{on}^{2D}$ of 0.0041 ± 0.0009 (motor/micrometer$^{-2}$)-s$^{-1}$ in AMPPNP was similar to that in ATP, consistent with the motor on-rates being identical in the 2 nucleotides. Thus, we have directly measured the bimolecular association rate constant for membrane-bound motors binding to MTs. As shown below, this parameter allows one to predict the travel distance of a vesicle with known size, motor number (from which motor density can be calculated), and motor $k_{off}$.

**Motor Attachment Is Not Limited by Membrane Diffusion.** The accumulation of membrane-bound motors on the MT can be considered as 2 sequential steps—motor diffusion ($k_{diffusion}$) into a binding zone near the MT ($A_{attach}$), followed by motor attachment to MT ($k_{attach}$) from this binding zone (Fig. 1L). Depending on the diffusion constant and distance covered, $k_{on}^{2D}$ could in principle be determined by either the motor diffusion rate or the motor association rate when near the MT. Because different vesicle compositions are known to have different lipid compositions (16, 17, 20), motor diffusivity could be a potential regulator of motor activity in cells.

To investigate whether diffusion or binding is rate-limiting for motor accumulation, we decreased the motor diffusion constant by incorporating 30 mol% cholesterol (the maximum amount under our conditions without membrane phase separation) into the POPC lipid bilayer. Fluorescence recovery after photobleaching (FRAP) measurements indicated that cholesterol incorporation resulted in a 3.8-fold decrease in the lipid diffusion coefficient from 0.95 ± 0.14 μm$^2$/s to 0.25 ± 0.03 μm$^2$/s with cholesterol (mean ± SD; n = 6 bilayers for each; Fig. 3A, SI Appendix, Table S1, and Movie S2). To ensure that the FRAP measurements accurately reflected the diffusivity of motors in the membrane across different motor densities, we measured motor diffusion coefficients by single-particle tracking in spiking experiments where only a small fraction of motors on the bilayer were labeled with GFP (SI Appendix, Fig. S2 and Table S1). For the control POPC membrane, the single-molecule diffusion constant was 0.93 ± 0.03 μm$^2$/s at ~40 motors/μm$^2$ and 0.87 ± 0.02 μm$^2$/s at ~250 motors/μm$^2$ (mean ± 95% confidence bound of MSD fitting; n = 193 and 271, respectively). Thus, the single-molecule diffusion constants are in good agreement with the FRAP results and do not vary with motor density. Addition of 30% cholesterol decreased $D$ to 0.46 ± 0.01 μm$^2$/s at ~60 motors/μm$^2$ and 0.53 ± 0.01 μm$^2$/s at ~340 motors/μm$^2$ (n = 301 and 254, respectively). This 2-fold decrease in diffusivity measured by single-molecule tracking was less than the ~4-fold decrease measured by FRAP. In similar single-particle
tracking experiments, it was shown that single-motor diffusion coefficients have a broad distribution (21, 22). Because our measurement technique involved prebleaching a region of interest and tracking motors diffusing into the bleached area, we hypothesize that the diffusion constant in the cholesterol experiments preferentially selects for faster diffusing motors and hence may overestimate the mean single-molecule diffusion constant. Nonetheless, our measurements confirmed that incorporating cholesterol into the lipid bilayers effectively reduced motor diffusivity.

We next quantified motor accumulation rate as a function of motor density in 2 mM ATP or AMPPNP on lipid bilayers containing 30% cholesterol (Fig. 3B). Addition of cholesterol into the membrane did not alter the motor attachment rate constant ($k_{\text{on}}$) to 0.0033 ± 0.0017 (motor/$\mu$m$^2$)$^{-1}$s$^{-1}$ in ATP, and 0.0030 ± 0.0008 (motor/$\mu$m$^2$)$^{-1}$s$^{-1}$ in AMPPNP; Fig. 3 C and D). This result seems surprising but, on closer inspection, makes sense, as follows. If we assume that the zone from which motors can bind to the MT extends 50 nm on either side of the MT (roughly the kinesin tether length (23–25)), then from the 1D diffusion equation $x^2 = 2Dt$, it should take motors an average of 1.3 ms (control) or 3 to 5 ms (plus cholesterol) to diffuse into and out of the zone. This times convert to rate constants orders of magnitude faster than 0.8 s$^{-1}$ kinesin-1 unbinding rate constant, meaning that following detachment (or equivalently following attachment), motor populations inside and outside the binding zone will rapidly equilibrate. We therefore conclude that, under our conditions, motor attachment to the MT is not limited by membrane diffusion. This suggests that kinesin-1 MT binding kinetics remain the same, regardless of membrane fluidity/ composition of cargos, unless they are organized into higher-order structures.

**Measured $k_{\text{on}}$ Predicts Kinesin-1 Can Explore 20 Tubulin Dimers during Attachment.** To better understand our observed motor accumulation kinetics and to relate them to the physiological case of spherical vesicles of varying diameters, we developed an analytical model of the motor accumulation process. Because the motor diffusion rate within the membrane is considerably faster than motor binding kinetics, we made the assumption that the pool of motors within the binding zone is in rapid equilibrium with the pool of motors outside the binding zone. From our measured parameters $k_{\text{on}}$, $\sigma$, the 2D bimolecular on-rate and the motor surface density, respectively, the flux of motors binding to the MT (in motors/second) is equal to $k_{\text{on}} \cdot \sigma$ (equivalent to $k_{\text{on}}$ [motor] in solution). If we consider only those motors within the binding zone of a given tubulin subunit, then we can calculate an equivalent motor flux onto the MT as the number of motors in the zone, $N$, multiplied by a first-order motor attachment rate constant, $k_{\text{attach}}$. In this case, the number of motors in the zone, $N$, is equal to $\sigma \cdot A_{\text{zone}}$, where $\sigma$ is the motor density and $A_{\text{zone}}$ is the area. Uniting these 2 representations of the motor flux onto the MT,

$$k_{\text{on,2D}} \cdot \sigma = k_{\text{attach}} \cdot \sigma \cdot A_{\text{zone}}.$$  \[3\]

Thus,

$$k_{\text{on,2D}} = k_{\text{attach}} \cdot A_{\text{zone}}.$$  \[4\]

Our experimentally determined $k_{\text{on,2D}}$ was 0.0034 (motor/$\mu$m$^2$)$^{-1}$s$^{-1}$. The first-order kinesin attachment rate constant, $k_{\text{attach}}$, has been previously calculated from a lipid vesicle system to be 4.7 s$^{-1}$ (10),

Fig. 3. $k_{\text{on,2D}}$ of membrane-bound motors is not controlled by membrane diffusion. (A) Example traces of fluorescence recovery after photobleaching (FRAP) measurement of lipid bilayers without (black) or with 30% cholesterol (gray). Diffusion coefficients were calculated as 0.96 and 0.25 $\mu$m$^2$/s, respectively, from single-exponential fitting. (Scale bar, 30 μm.) See SI Appendix, Fig. S2 for single-molecule diffusion estimates. (B) Motor accumulation rate constant versus kinesin-1 density in 2 mM ATP (blue) or 2 mM AMPPNP (red) in the presence of 30% cholesterol in the membrane. Each data point represents the mean of 8 to 83 measurements. Error bars indicate SEM. (C and D) Summary of $k_{\text{on,2D}}$ (C) and $k_{\text{off}}$ (D) of membrane-bound kinesin-1 motors under different membrane compositions and nucleotide conditions. Error bars indicate 95% confidence bound of fit.
from a DNA scaffold to be 4.6 s\(^{-1}\) (12), and from a bead system to be 5 s\(^{-1}\) (26). Although the 2D lipid bilayer system is a third geometry, we make the tentative assumption that the first-order association rate constant also applies here. Thus, we can calculate an estimate for the area around a given tubulin subunit from which motors can bind as \(A_{\text{zone}} = 680 \text{ nm}^2\). Our truncated kinesin-1 has a contour length of roughly 50 nm. Thus, if a model is used in which every motor within a contour length of a given tubulin is able to bind, an approach taken by others (5, 27), \(A_{\text{zone}}\) is expected to be \(\sim 8,000 \text{ nm}^2\), considerably larger than our estimate. If motor reach is the determining factor for how many motors can productively interact with a tubulin subunit, then from a symmetry argument, the area of motors accessible to a given tubulin subunit should be equivalent to the area of tubulin subunits accessible to a given motor. Thus, we can interpret the \(A_{\text{zone}}\) of 680 \text{ nm}^2 as kinesin-1 being able to stretch \(\sim 15 \text{ nm}\) (a circle with \(r = \sqrt{680 / \pi}\)), or equivalently, being able to explore \(\sim 20\) tubulin subunits [680 \text{ nm}^2/(8 \text{ nm} \times 4 \text{ nm})]. This reach is considerably smaller than the motor’s contour length of 50 nm, but it is in good agreement with the distance that kinesin-1 holds its cargo from the MT, previously measured to be \(\sim 17 \text{ nm}\) (23, 28).

**Slow Attachment Predicts High Motor Densities for Long-Range Vesicle Transport.** Achieving run lengths greater than the single-motor distance requires multiple motors on a cargo simultaneously binding to the MT, such that when one motor dissociates, others are there to continue transport. Using the kinetic parameters measured here, we carried out simulations to predict the number of kinesin-1 motors required to achieve long-range transport of vesicles of varying diameters. The vesicle motor density, \(\sigma\), was defined as the number of motors on the vesicle divided by the membrane surface area of the vesicle. The flux of vesicle-bound motors binding to the MT was defined as \(k_{\text{on}}^{2D}\), and the flux of motors detaching from the MT was defined as \(k_{\text{off}}\) times the number of MT-bound motors. A naïve prediction of this system is that for vesicles considerably smaller than the motor contour length, every motor can access the MT, so having multiple motors on a vesicle leads to longer run lengths. Consistent with this prediction, for vesicles of 30 nm in diameter, 2 motors are sufficient to double the run length, and 6 motors can carry the vesicle for 10 \mu\text{m} on average (Fig. 4A). However, analogous to the slow accumulation in the SLB system, we found that, for larger cargos, achieving multimicron travel distances requires higher motor numbers. For instance, a 100-nm vesicle needed \(\sim 35\) kinesin-1 motors to travel 10 \mu\text{m}, and a 500-nm vesicle required \(\sim 800\) motors to travel the same distance (Fig. 4A). Further insight into the underlying motor dynamics can be seen by comparing the average number of motors engaged with the MT (Fig. 4B) to the average travel distances (Fig. 4C) for different vesicle sizes and total motor numbers. It can be seen that 10-\mu\text{m} travel distances are achieved when on average only \(\sim 3\) motors are engaged with the MT at any given time. The finding that tens to hundreds of motors per vesicle are needed to achieve a handful of engaged motors emphasizes that motor binding kinetics, rather than the total number of motors per vesicle, is the primary determinant of vesicle transport distance.

Although our prediction of high motor numbers per vesicle seems surprising, it is in fact consistent with a number of published optical trap experiments, where single-molecule activity is routinely achieved by incubating \(\sim 500-1,000\)-nm-diameter beads with a thousand-fold excess of motors (29, 30). For vesicles larger than the motor contour length, motor–MT interactions are naturally geometrically constrained; for instance, it has been calculated that for a 760-nm-diameter vesicle, only 4% of dynein randomly distributed on the surface can reach the MT, assuming a dynein contour length of 70 nm (5). Our conclusion that the reach distance for a motor is much less than its contour length further shifts this percentage down and provides a kinetic description of the process. In published work, smaller cargos were also found to have a similar requirement of high kinesin-1 copy numbers for long-distance transport. Using 100-nm-diameter beads, Beeg et al. (26) found that the run length only marginally increased when up to 73 motors were bound to the bead, whereas we predict 35 motors are sufficient to carry a 100-nm vesicle for 10 \mu\text{m} on average (Fig. 4A). Beeg et al. (26) also estimated that, on average, \(\sim 3\) motors were engaged at these motor concentrations, similar to our result in Fig. 4B, and supporting the idea that the motor attachment kinetics rather than the total number of motors bound to a vesicle is what controls transport distances.

The motor copy numbers that we predict based on our accumulation measurements are somewhat higher than previous measurements using purified neuronal vesicles and phagosomes. Using quantitative Western blots or photobleaching, it was estimated that \(\sim 90\text{-nm vesicles contain on average 3 to 10 dynein, 1 to 3 kinesin-1, and 2 to 6 kinesin-2 motors (6, 31). One hypothesis to account for these low motor numbers is that motors from different families have different binding kinetics that could improve their transport efficiency in teams and thereby reduce the number of motors required for long-range transport. For instance, kinesin-2 has been shown to have a 4-fold faster \(k_{\text{on}}\) compared to kinesin-1, suggesting it may play a tethering role to maximize attachment of a vesicle to the MT (12). Also, activated mammalian dynein–dynactin–BicD2 (DDB) complexes have a \(k_{\text{off}}\) on the order of 0.04 s\(^{-1}\) (32), meaning that slowly detaching DDBs can hold a vesicle near the MT, enabling kinesins that detach to rebind and continue bidirectional transport. To test this hypothesis, we ran simulations where we varied \(k_{\text{on}}\) or \(k_{\text{off}}\).
and found that transport efficiency increased drastically with either a faster $k_{on}$ or a slower $k_{off}$ (Fig. 4C). If the motor had a 3-fold faster $k_{on}$ then instead of 35 motors, only 13 motors were needed to carry a 100-nm vesicle for 10 μm. A 3-fold slower $k_{off}$ had an even more prominent effect—only 9 motors were sufficient to carry the vesicle for the same distance. Motor clustering into membrane subdomains is another factor that could enhance long-distance vesicle transport. For instance, in late phagosomes, dynein has been shown to cluster into microdomains (5), which is expected to increase its $k_{on}$ dramatically because motors no longer diffuse in the membrane and their clustering significantly increases the local motor density. In analogy to motor clustering within lipid microdomains, motors closely packed on DNA scaffolds generally have long run lengths with low motor copy numbers. For instance, 2 kinesin-1 motors spaced 15 or 23 nm apart on a DNA scaffold doubled the run length (12, 33), and 4 kinesin-1 spaced 23 nm apart (33) or 7 kinesin-1 spaced 28 nm apart (34) exhibited 7-fold longer run lengths. These long run lengths can be explained by the fact that the scaffold geometries ensure that all of the motors fall within the area $A_{zone}$, where every motor is able to reach the MT.

Conclusions

Organelles and other membranous cargos need to travel tens of micrometers or longer to reach their cellular destinations, which is achieved by a network of motors that only travel several micrometers individually. The distance that a cargo can travel is ultimately determined by the race between attachment of the free motors and detachment of the bound motors. In this study, we dissected 4 key parameters in this kinetic process. From the motor accumulation on a lipid bilayer, we measured $k_{off}$, which matches with previous single-molecule studies, and the 2D bimolecular association rate constant, $k_{2D}$. This on-rate parameter encompasses the following: 1) the membrane diffusion rate constant $k_{diffusion}$, 2) the binding zone $A_{zone}$ within which motors can access the MT, and 3) $k_{attach}$ the first-order attachment rate constant when motors are within the binding zone. $k_{on}$2D remained unchanged when membrane diffusivity was reduced by cholesterol, indicating that motor attachment is not limited by membrane diffusion and suggesting that changes in membrane fluidity are not an effective mechanism by which cells can regulate transport properties of different vesicle cargos by kinesin-1. Using the reported value of $k_{attach}$ our theoretical work suggests an $A_{zone}$ smaller than that predicted by the motor contour length, and one that is close to the area of ∼20 tubulin dimers. This small zone of interaction explains the intrinsically slow binding of kinesin-1 to the MT and the prediction that relatively high motor densities are required for long-range vesicle transport. This work suggests teamwork between dissimilar motors can enhance vesicle transport, and leaves open the possibility that some vesicles achieve long-distance transport by clustering motors in membrane microdomains or through scaffold proteins. As suggested from recent work on dynein (5), this clustering may be a mechanism to regulate vesicle moving directionality during bi-directional transport in cells.

Materials and Methods

Protein Constructs and Purification. The K560GFP–AviC construct was made by inserting the biotin ligase consensus sequence (AviTag) (13) between the eGFP tag and the 6x His tag in a previously described K560GFP construct (12). Insertions were carried out using Q5 site-directed mutagenesis (New England Biolabs). Motors were expressed polyclonally with BirA biotin ligase, in BL21 (DE3) bacteria (New England Biolabs), and purified by affinity chromatography, as previously described (12, 13, 35). Motor concentration was quantified by GFP absorbance or fluorescence at 488 nm.

Formation of SLBs. POPC, DSPE-PEG(2000)-Biotin, and cholesterol were purchased from Avanti. Lipids were dissolved in chloroform and mixed in desired molar ratio, 1,2-Dioleoyl-sn-glycerol-3-phosphoethanolamine labeled with Atto 647N (Atto 647N DOPE) (Sigma) was incorporated into all lipid bilayers for visualization. Lipid composition without cholesterol was POPC:DSPE-PEG(2000)-Biotin:Atto 647N DOPE at 99.0:1.0-0.6:0.05, and the composition with cholesterol was POPC:cholesterol:DSPE-PEG(2000)-Biotin:Atto 647N DOPE at 69:30:0.1-0.6:0.05. The bulk of chloroform in the lipid mixture was evaporated in a rotary evaporator for 1.5 h. Lipids were left under vacuum for another 3 h to remove any trace of chloroform. The dry lipid film was rehydrated in BRB80 (80 mM Pipes, 1 mM EGTA, 1 mM MgCl₂; pH 6.9) to a final lipid concentration of 0.5 mg/mL, and the lipid suspension was subjected to a freeze-thaw cycle in liquid nitrogen and warm water bath. Small unilamellar vesicles (SUVs) were formed by passing the lipid solution 11 times through a 100-nm polycarbonate membrane, followed by 21 times through a 30-nm membrane, using a minitextruder (Avanti).

Glass coverslips (#1.5; 24 × 30 mm; Corning) were cleaned as previously described (36). Coverslips were boiled in 7x detergent (MP Biomedicals) diluted 1:7 with 18.2-MΩ water for 2 h. Coverslips were then rinsed thoroughly with 18.2-MΩ water, blown dry with nitrogen, and annealed at 550 °C for 6 h. Coverslips were cleaned by a plasma cleaner (Harrick Plasma) immediately before formation of SLBs. Polydimethylsiloxane (PDMS) spacers were made using Sylgard 184 silicone elastomer kit (Dow Corning). Cured PDMS was cut by a biopsy punch (Acuderm) to make spacers 6 mm in inner diameter and 2-mm thick that were adhered to clean coverslips. SUVs (50 μL) were added to the well and incubated for 10 min, followed by thorough wash in BRB80 to remove excess SUVs.

Accumulation Assay. Taxol-stabilized MTs were polymerized from bovine brain tubulin, as described previously (12–14, 35). Rhodamine-labeled MTs (rhodamine:unlabeled, 1:3) were used in experiments in Fig. 1C; unlabeled MTs were used otherwise. MTs were sheared by passing twice through a 30-g needle. Motor-functionalized bilayers were formed by binding preformed kinesin–NeutrAvidin complexes to biotinylated lipid bilayers, as follows. Kinesin (200 nM) was incubated with 2 μM NeutrAvidin (Thermo Scientific) in BRB80 containing 100 μM Taxol and 1 mM DTT for 10 min at room temperature (RT). Excess of NeutrAvidin ensured that all biotinylated motors were occupied, without cross-linking of motors. To remove excess NeutrAvidin, the solution was incubated 10 min with 1 μM MT and centrifuged for 10 min in an Airfuge (Beckman Coulter); inactive motors and excess NeutrAvidin in the supernatant were discarded. The pellet containing MTs with bound kinesin–NeutrAvidin (K–NA) was resuspended in motor buffer (1 μM Taxol, 2 mM ATP, 20 mM D-glucose, 1 mM DTT in BRB80), incubated for 10 min at RT to release active motors, followed by an Airfuge spin to remove MTs with irreversibly bound motors. SLBs were equilibrated with motor buffer; 50 μL of K–NA solution was then introduced, followed by a 10-min incubation to allow motors to bind to the SLB. Excess motors were removed by a wash of motility buffer (1 μM Taxol, 2 mM ATP or AMPPPNP, 1 mM DTT, 40 mM D-glucose, 0.02 mM glucose oxidase, 0.008 mg/mL catalase in BRB80), MTs (16–32 nM) in motility buffer were introduced immediately before imaging. Accumulation of GFP-labeled motors was imaged using a Nikon TE2000 TIRF microscope (except for Fig. 1C, which was captured using an epifluorescence microscope) at 10 to 11.4 fps, as described previously (14).

Motor Density Quantification and Single-Motor Diffusion Determination. Motor densities were calculated by directly counting motor densities by single-molecule TIRF at low motor densities and extrapolating up to high motor densities using the mean GFP fluorescence intensity of the bilayer. Motor densities were controlled by different methods at low and high motor densities. For higher motor densities, corresponding to 40 to 250 motors/μm² in Fig. 2, and 57 to 340 motors/μm² in Fig. 3B, motor densities were controlled by varying the amount of DSPE-PEG(2000)-Biotin (0.1 to 0.6%) in the SLBs and incubating the SLBs with saturating amount of K–NA. Because it was difficult to measure extremely small amount of lipids accurately, a statistical method was used to achieve low motor densities. SLBs containing 0.1% DSPE-PEG(2000)-Biotin were incubated with motor-free NeutrAvidin spiked with varying amounts of K–NA, so that only a fraction of DSPE-PEG(2000)-Biotin was occupied by K560GFP–AviC. To ensure surface motor densities scaled up as we expected, we measured the mean GFP intensities from motors at varying surface motor densities under constant TIRF illumination and exposure time. The fluorescence intensity scaled linearly with equivalent biotin concentration in the membrane [DSPE-PEG(2000)-Biotin (%) × motor spiking ratio; SI Appendix, Fig. 53]. This approach allowed us to use mean bilayer fluorescence to extrapolate from low densities where motors could be directly counted, up to the higher densities used for accumulation assays.
To quantify the actual surface motor densities, we used single-molecule TIRF to directly count motor densities in spiking experiments where 1/50 of the NeutrAvidin on membranes containing 0.1% DSPE-PEG(2000)-Biotin were fully occupied. We used 41/26570 m2 and 57/26570 m2 per 0.1% DSPE-PEG(2000)-Biotin for SLBs without and with 30% cholesterol, respectively, to extrapolate to other motor densities.

To quantify the single-molecule motor diffusion constant, we attached K560GFP-AviC spiked with small amounts of K560GFP-AviC to the SLBs, as follows. SLBs were first incubated with motor-free NeutrAvidin spiked with K560GFP-AviC–NA. Complexes. After removing the unbound proteins, SLBs were then incubated with saturating level of K560GFP-AviC to occupy all of the NeutrAvidin sites. In order to remove any immobile spots on the surface that would interfere with tracking, and to reduce the number of diffusing molecules to avoid overlaps between traces, we prebleached the field of view before taking a video. Motor diffusion was then imaged by TIRF microscopy at 10 fps.

FRAP. To obtain sufficient signal-to-noise ratio for FRAP measurement, 0.5 mol% Atto 647N DOPE was incorporated into SLB samples. Images were captured using a Nikon Eclipse Ti microscope equipped with a Plan Apo 10× DIC N1 objective and an attached digital complementary metal-oxide semiconductor (CMOS) camera (ORCA-Flash 4.0 V2; Hamamatsu) in conjunction with N5-Elements (Nikon) software. SLBs were excited with a 640-nm light source (Aluxa; Lumencor). A 15-mW, 561-nm laser (LU-N3 Laser Unit; Nikon) equipped with a Bruker Miniscanner was used to bleach Atto 647N DOPE at 50% output power for 3 s. The laser beam had an effectively cylindrical profile with a diameter of 30 μm. To minimize photobleaching during recovery, images were captured immediately after bleaching every 40 to 60 ms for 2 s, then every 500 ms for 10 s, followed by every 3 s for 2 min, and finally switched to every 30 s. Data analysis was carried out as previously described (36), using a correction factor of 1.

Data Analysis. Accumulation image sequences were analyzed in Fiji (37). The trace that a newly landing MT glided along was tracked manually, and the GFP intensity profile along the trace was plotted over time. The frame that the MT landed was defined by the slope maximum on a plot of average GFP intensity along the trace versus time. After background correction, the trace was fitted by a single-exponential function from which \( k_{off} \) was obtained. A weighted (by inverse of SEM) linear regression between \( k_{off} \) and surface motor density by linear least-square fitting was carried out in MATLAB (The MathWorks).

One of single motors was tracked using FIESTA (38). Displacement data of all trajectories were calculated for discrete lag times, and the displacement data were cumulated to calculate the average MSD for each time point. To obtain motor diffusion coefficients, the first 10 points of the MSD were fitted with a line weighted by the inverse of SEM.

Simulation of Vesicle Transport. Vesicle transport was simulated by modifying a MATLAB code that was previously used to simulate single-molecule runs (35). The vesicle diameter, D, and total motor number, \( N \), were defined at the beginning of the simulation. Each state was defined by the number of engaged motors, \( i \). The transition rate from state \( i \) to state \( i + 1 \) was defined as \( k_{on} (N-I)/(D+4D(D+2)) \). The transition rate from state \( i \) back to state \( i-1 \) was defined as \( k_{off} \). Vesicle dwell times on the MT were simulated based on the transition matrix. Average vesicle transport distances were calculated by multiplying the simulated dwell time by the kinesin-1 velocity of 600 nm/s (13).

Data and code are available to readers in the Pennsylvania State University institutional repository, ScholarSpace, https://doi.org/10.26207/ap7-b307.

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